

Current Drug Metabolism,
Volume 17 , Issue 8 , 2016

New Metal based nanoparticles coated with biomolecules for targeted therapy



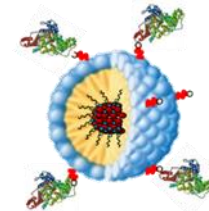
Dr. Laura Zaccaro

Istituto di Biostrutture e Bioimmagini-CNR-Napoli

lzaccaro@unina.it

Scuola di Bioinorganica, CNR-Roma 13-15 febbraio 2019





Overview

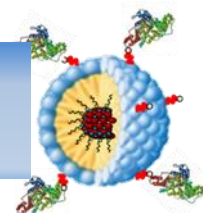
Cancer and Targeted therapy





Nanotechnology in Targeted Therapy

Magnetic and Gold Nanoparticles

New Metallic Nanoparticles as Theranostics

Cancer and Targeted Therapy



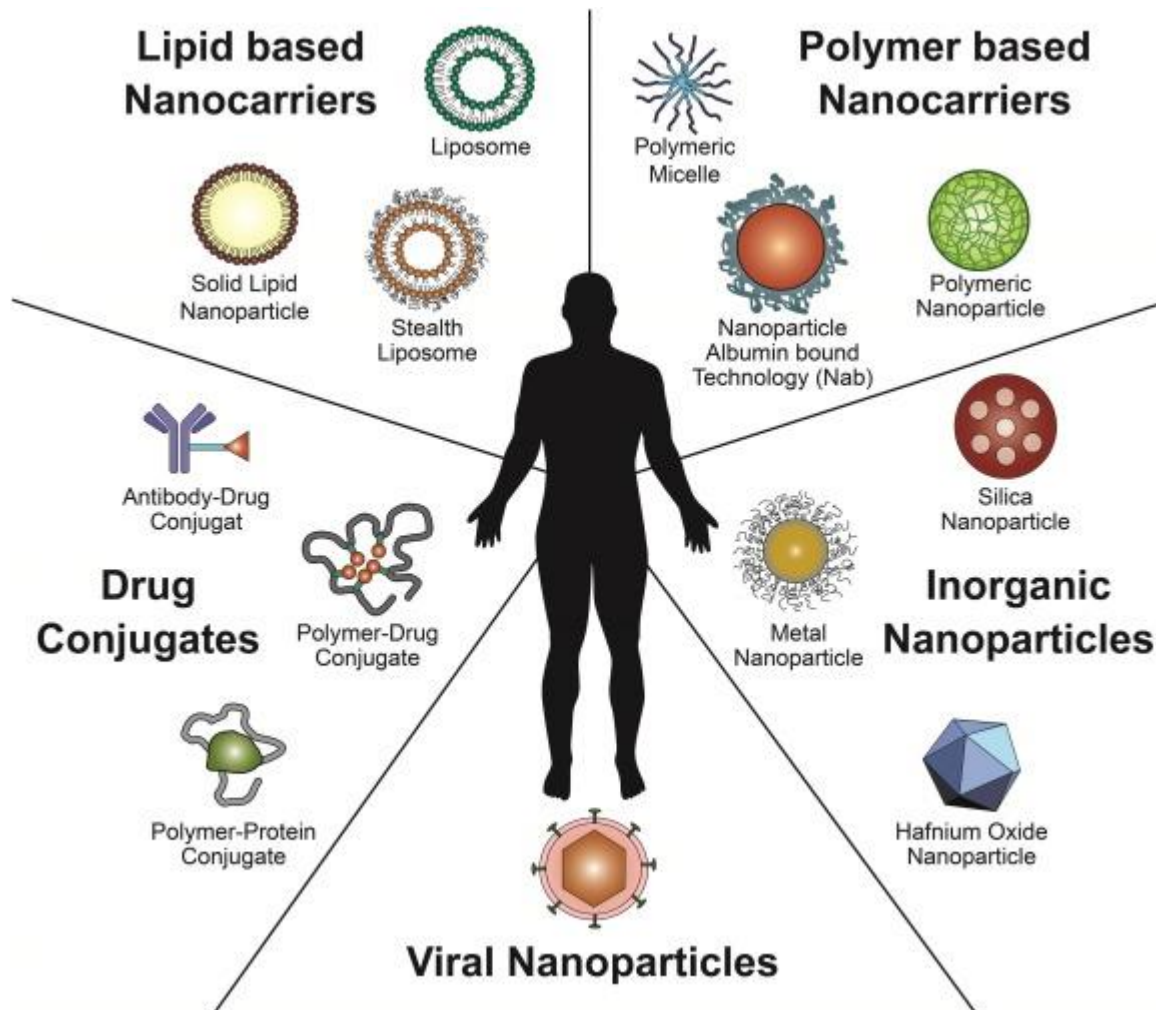
-  Cancer is currently one of the most difficult global healthcare problem
-  Standard treatments include chemotherapy, radiation, and surgery, but the effects of these procedures may damage not only the tumor tissue but also normal tissue.
-  Cancer recurrence is believed to be one of the major reasons for the failure of cancer treatment strategies.
-  Current problems in treating cancer include rapid drug clearance and biodegradation, and limited targeting.

The advent of nanomedicines have led significant advances in the field of targeted therapy

Advantages of therapeutic nanoparticles

- Revert unfavorable physicochemical properties of bioactive molecules to desirable biopharmacologic profiles;
- Improve delivery of therapeutics across biological barriers and compartments;
- Control release of bioactive agents;
- Enhance therapeutic efficacy by selective delivery of therapeutics to biological targets;
- Perform theranostic functions by combining multimodal imaging and simultaneous diagnosis and therapy into multifunctional nanoplatforms.

Nanomedicines in cancer treatment



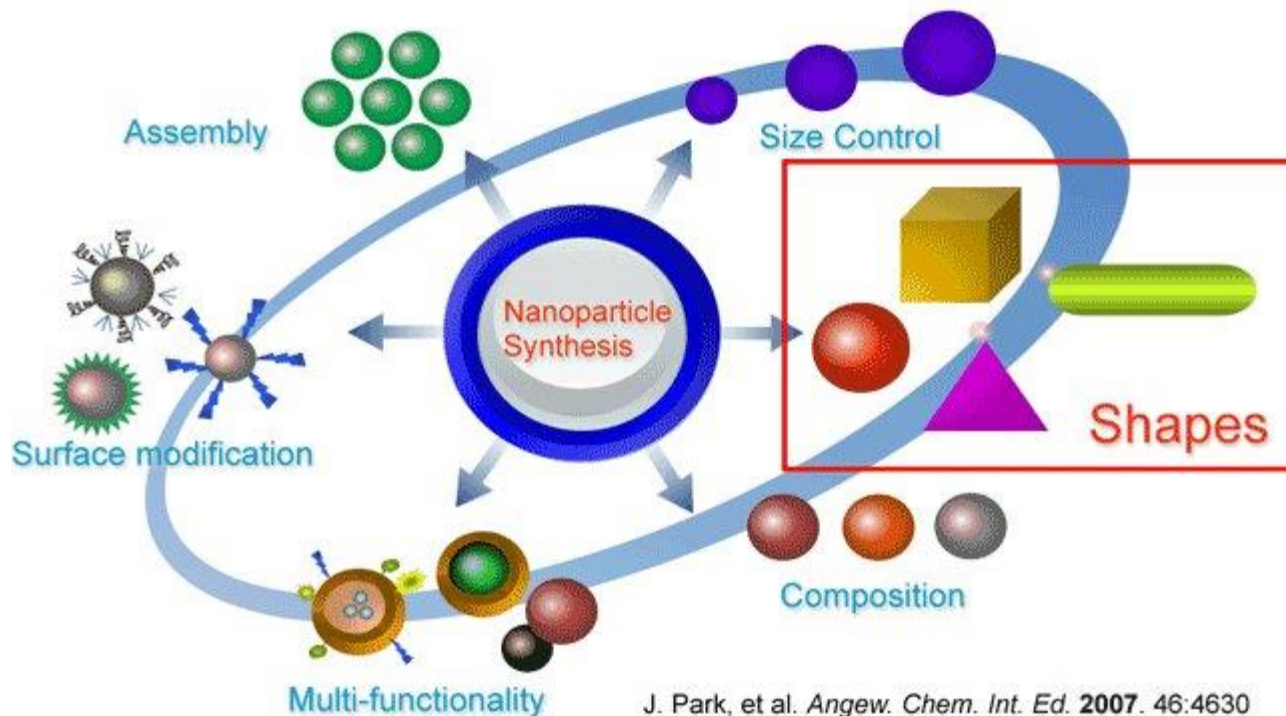
Approved nanomedicines in the clinic

| Year approved | Name | Type | Active drug | Diameter (references) | Type of cancer |
|--------------------------|-----------------------|----------------------------|--|-----------------------|---|
| Japan (1994) | Zinostatin stimalamer | Polymer protein conjugate | Styrene maleic anhydride neocarzinostatin (SMANCS) | * | Renal cancer |
| FDA (1995) EMA (1996) | Doxil/caelyx | Liposome (PEGylated) | Doxorubicin | 80–90 nm [82] | HIV-associated Kaposi's sarcoma, ovarian cancer, metastatic breast cancer, multiple myeloma |
| FDA (1996) | DaunoXome | Liposome (non-PEGylated) | Daunorubicin | 45 nm [83] | HIV-associated Kaposi's sarcoma |
| Taiwan (1998) | Lipo-Dox | Liposome | Doxorubicin | 180 nm [84] | Kaposi's sarcoma, breast and ovarian cancer |
| FDA (1999) | DepoCyt | Liposome | Cytosine arabinoside (cytarabine) | 10–20 μ m [84] | Neoplastic meningitis |
| EMA (2000) | Myocet | Liposome | Doxorubicin | 190 nm [84] | Breast cancer |
| FDA (2005) EMA (2008) | Abraxane | Nanoparticle albumin bound | Paclitaxel | 130 nm [27] | Advanced non-small-cell lung cancer, metastatic pancreatic cancer, metastatic breast cancer |
| FDA (2006) | Oncaspar | PEG protein conjugate | L-Asparaginase | 50–200 nm [84] | Leukemia |
| South Korea (2007) | Genexol-PM | PEG-PLA polymeric micelle | Paclitaxel | 20–50 nm [85] | Breast cancer, Lung cancer, Ovarian cancer [126] |
| EMA (2009) | MEPACT | Liposome (non-PEGylated) | Mifamurtide | * | Osteosarcoma |
| EMA (2010) | NanoTherm | Iron oxide nanoparticle | – | 20 nm [86] | Thermal ablation glioblastoma |
| FDA (2012) | Marqibo | Liposome (non-PEGylated) | Vincristine | 100 nm [87] | Philadelphia chromosome negative acute lymphoblastic leukemia |
| FDA (2015) | MM-398 (Onivyde) | Liposome (PEGylated) | Irinotecan | 80–140 nm [88] | Metastatic pancreatic cancer (2nd line) |

* Data could not be found

Tran et al. Clin Trans Med (2017) 6:44

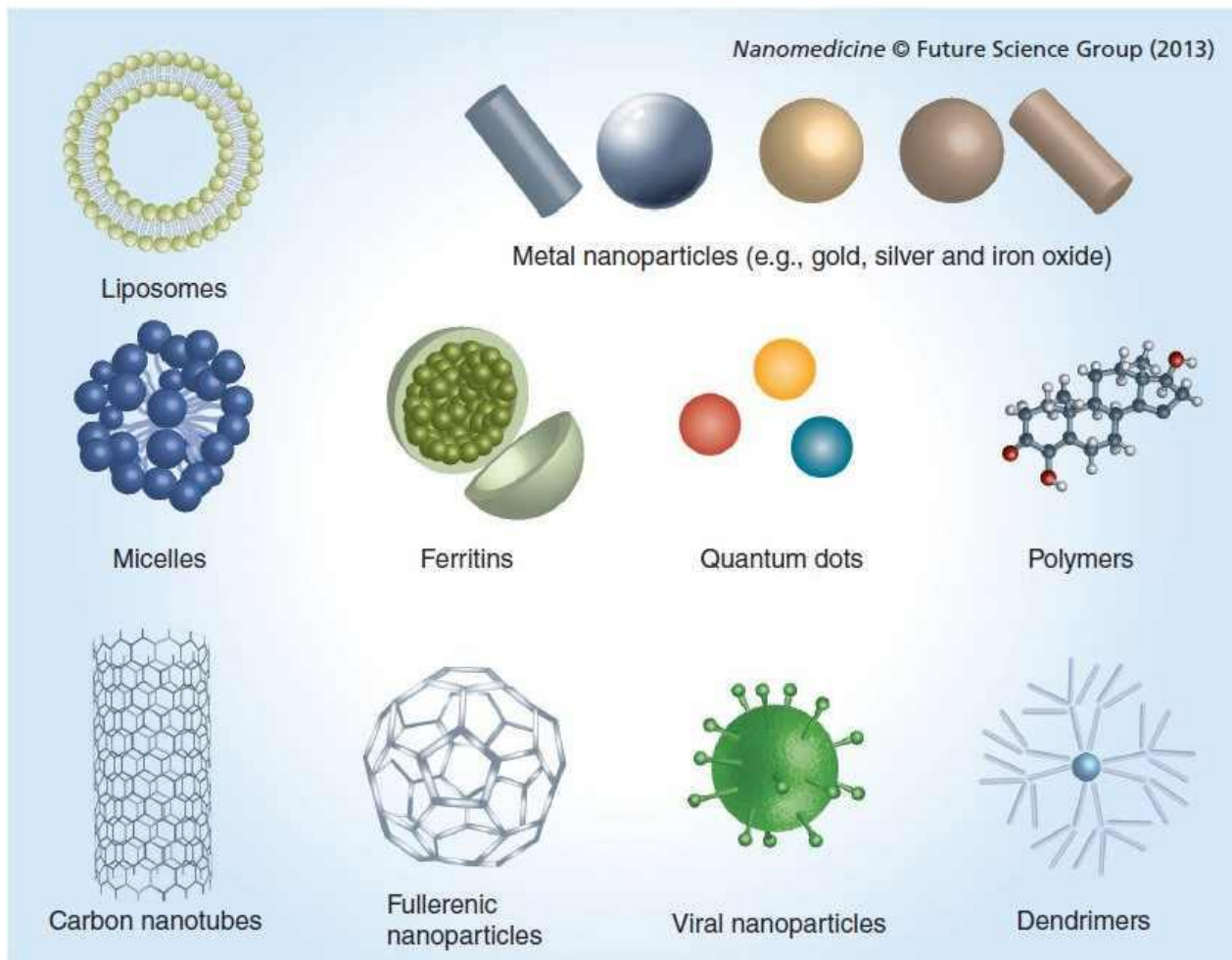
Nanoparticle Properties



J. Park, et al. *Angew. Chem. Int. Ed.* **2007**. 46:4630
 S. Kwon & T. Hyeon *Acc. Chem. Res.* **2008**. 41:1696

The properties of nanocarriers, including their nanoscale sizes, high surface-to-volume ratios, favorable drug release profiles, and targeting modifications, can allow them to better reach target tumor tissue and release drugs in a stable, controlled manner

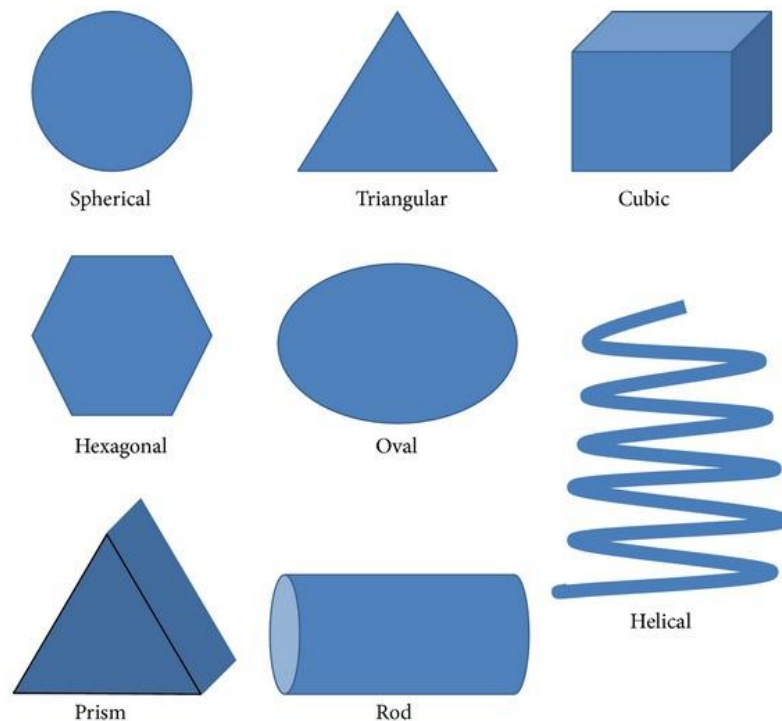
Surface features



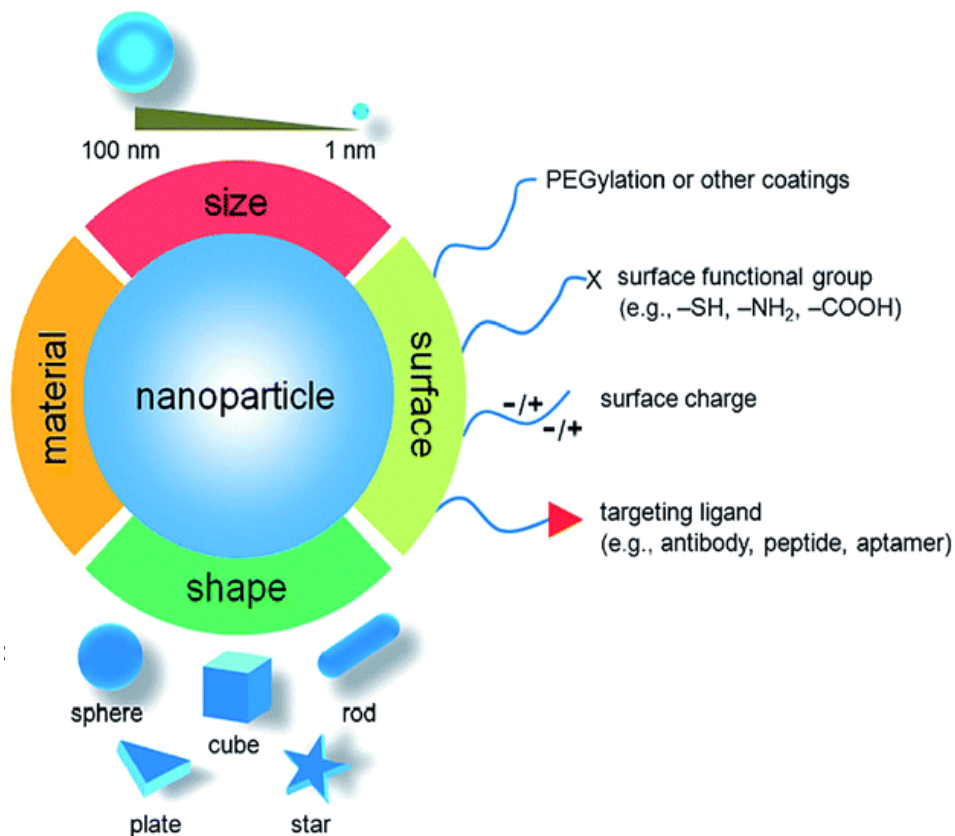
Nanoparticle size and shape

The shape and the size have high impact on:

- ❖ cell internalization mechanism
- ❖ high surface-to-volume ratios
- ❖ Optical and magnetic properties

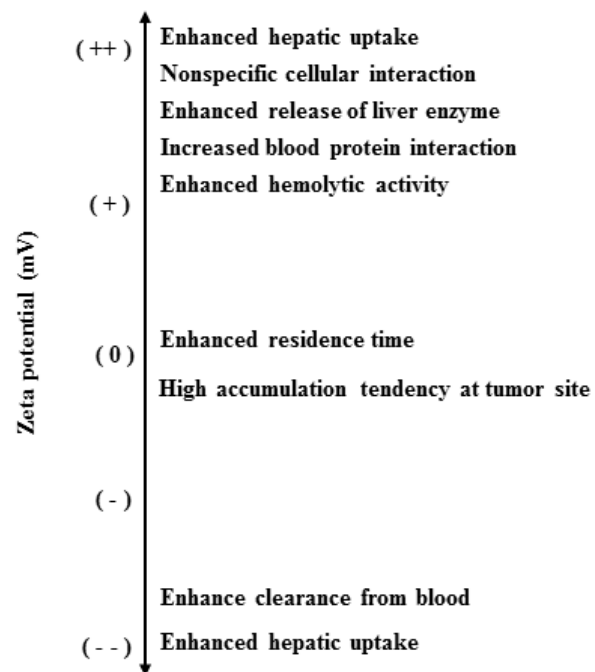


Surface features

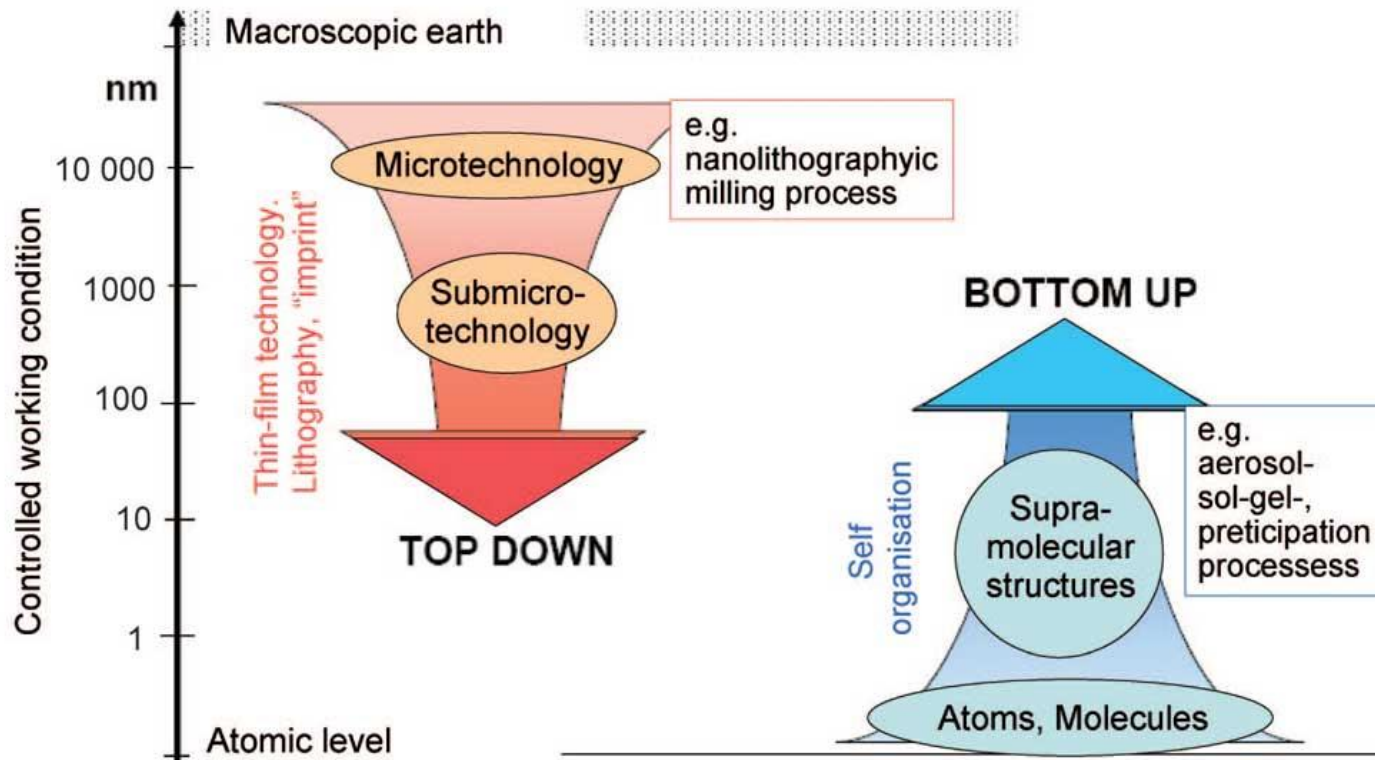


RSC Adv., 2016, 6, 82596–82615

Nanoparticle surface charge based effects



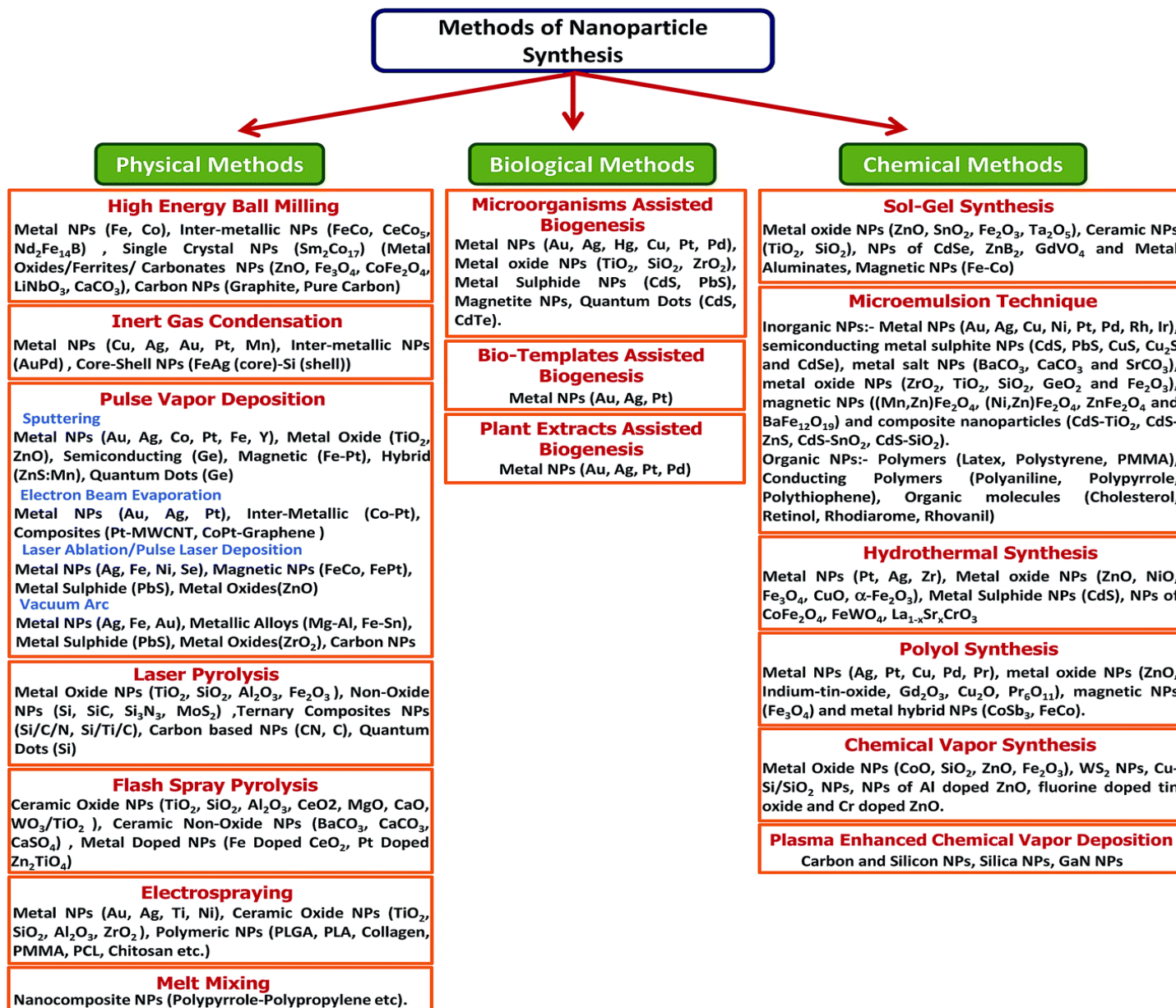
Synthetic methods



(Image: Laboratory for Micro and Nanotechnology, Paul Scherrer Institut)

Top-down or destructive method is the reduction of a bulk material to nanometric scale particles. Mechanical milling, nanolithography, laser ablation, sputtering and thermal decomposition are some of the most widely used nanoparticle synthesis methods

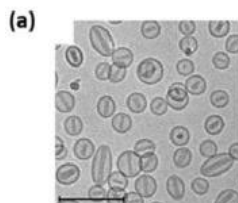
Bottom-up or constructive method is the build-up of material from atom to clusters to nanoparticles. Sol-gel, spinning, chemical vapour deposition (CVD), pyrolysis and biosynthesis are the most commonly used bottom-up methods for nanoparticle production.



Clinically relevant nanoparticle types

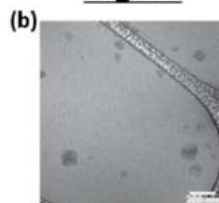
(Black: Approved Application, Red: Application in a Current Clinical Trial)

Organic



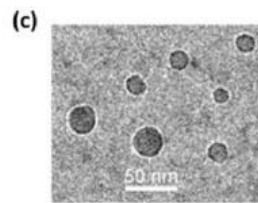
Liposomes:

Small-molecule Cancer Drugs
Ultrasound Contrast Agents
Vaccines
Anesthetics
Fungal Treatments
Macular Degeneration
Gene Therapies
Bacterial Infections
Inflammation (Arthritis)
Graft versus Host Disease



Protein-Based:

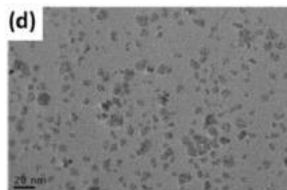
Small-molecule Cancer Drugs
Ultrasound Contrast Agents



Polymeric/Micelle:

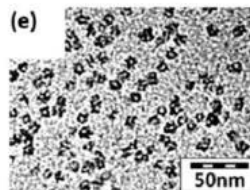
Small-molecule Cancer Drugs
Acute Radiation Syndrome

Inorganic



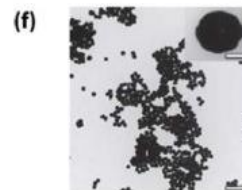
Iron-Oxide:

Anemia Therapies
Imaging Applications
Thermal Ablation of Tumors



Silica:

Cancer Imaging



Gold:

Thermal Ablation of Tumors

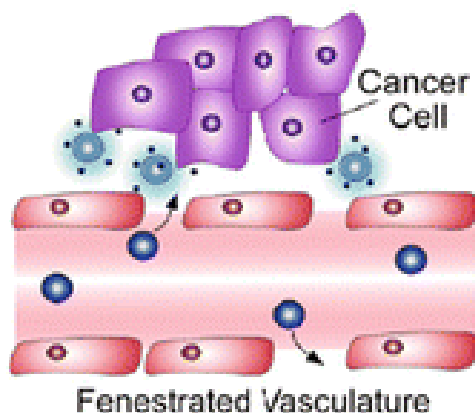
Advantages versus disadvantages

| Types of carriers | Advantages | Disadvantages |
|---|---|--|
| Liposomes | Biocompatible Longer duration of circulation | May trigger immune response |
| Carbon nanoparticles | Amphiphilic Multiple functions Chemical modification Water soluble and biocompatible Efficient loading | Toxicity |
| Polymeric micelles | Efficient carrier system for hydrophilic drug Biodegradable, self-assembling and biocompatible Potential targeting Functional modification | Occasional cytotoxicity Need of surface modifications |
| Dendrimers | Uniformity in size, shape and branch length Tuned pharmacokinetics and biodistribution Increased surface area, increased loading Targeting is achieved | Complex synthetic route |
| Metallic nanoparticles Gold nanoshells | Uniformity in size, shape and branch length Tuned pharmacokinetics and biodistribution Increased surface area, increased loading Targeting is achieved | Toxicity |

Lambert M. et al , 2014, Expert.Opin.Drug Deliv, 11, 1087

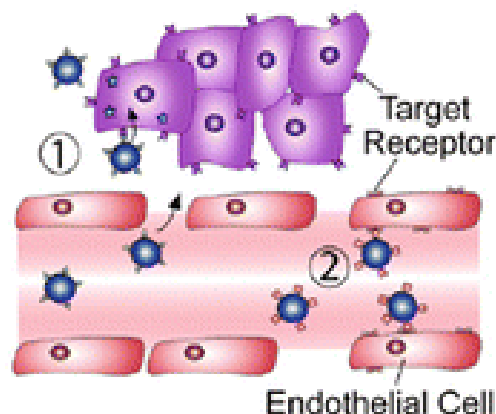
Targeting for nanoparticle delivery

a Passive Targeting



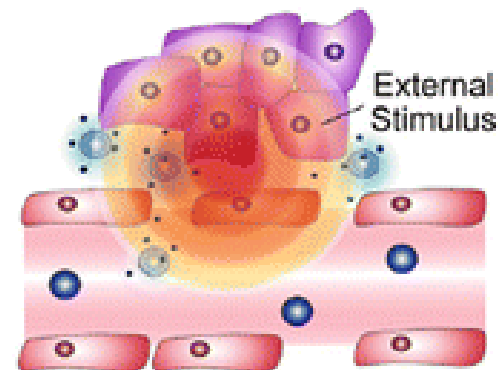
Passive targeting relies on the leaky vasculature that is exhibited by tumors, allowing nanoparticles to travel through the fenestrations and reach tumors.

b Active Targeting



Active targeting can be used when nanoparticles have ligands on their surface that can recognize and bind receptors that are overexpressed on tumor cells.

c Triggered Release



Tran et al. Clin Trans Med (2017) 6:44

Triggered release allows nanoparticles to conglomerate if exposed to an external stimulus such as a magnetic field or light

Active Targeting

Targeting nanoparticles to receptors or other surface membrane proteins overexpressed on target cells.

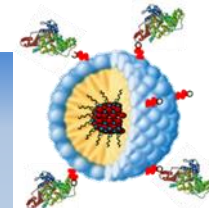
EGFR (epidermal growth factor) receptor overexpressed in malignant epithelial tumors as pancreatic and colorectal carcinoma

HER2 (human epidermal growth factor 2) receptor overexpressed in 25% of invasive cancer

PSMA (Prostate-specific membrane antigen) expressed on prostate cancer cells and on neovasculature of non prostate solid tumor

Transferrin receptor overexpressed on metastatic and drug resistant malignant cells

Integrin receptors overexpressed in activated neovessel and on cancer cell of solid tumors



Targeting ligands for active targeting

I. Antibody based targeting

B) Antibody fragment based targeting
single-chain anti-EGFR antibody (scFV)
Fab fragment

A) Monoclonal antibody based targeting
HER2/neu

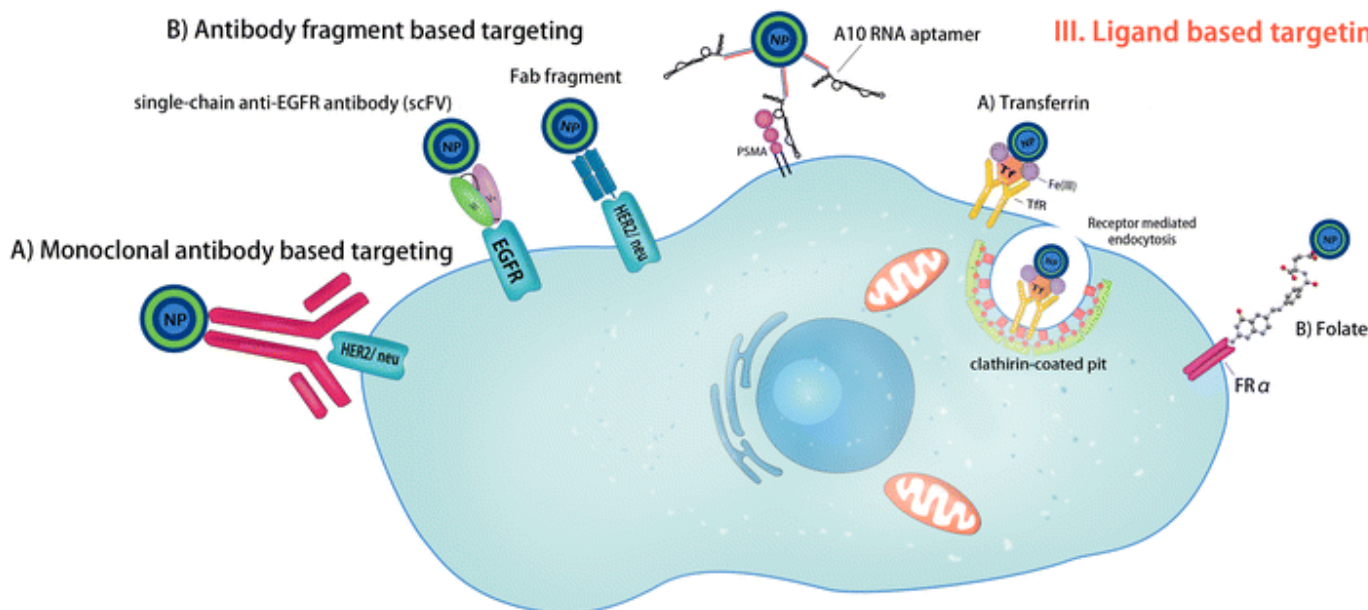
II. Aptamer based targeting

A10 RNA aptamer
PSMA

III. Ligand based targeting

A) Transferrin
TfR
Receptor mediated endocytosis
clathrin-coated pit

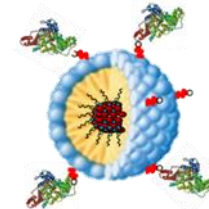
B) Folate
FR α



Bazak R et al. 2015, J cancer Res Clin Oncol, 141,769

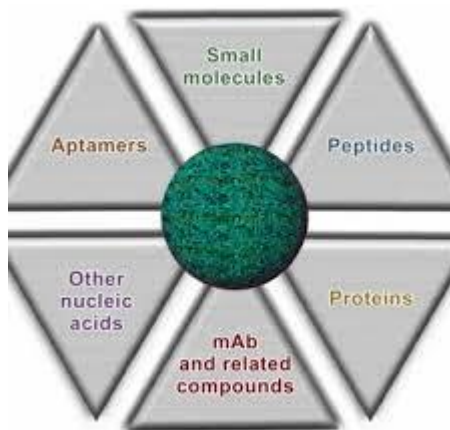
Numerous targeting ligands have been employed to actively target nanoparticles including antibodies, antibody fragments, aptamers, peptides and whole proteins

Targeted Nps for cancer therapy



BIND-014:nanoparticles loaded with docetaxel and decorated with urea-based Inhibitor to bind PSMA (Phase II clinical trials)

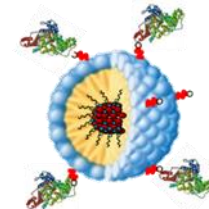
Nanoparticles (PLA/PEG) loaded with docetaxel and decorated with RNA A10-aptamer to bind PSMA



C-Dot: PEG- silica nanoparticles decorated with *i*RGD peptide

MBP-426, a scFv-transferrin-targeted liposome encapsulating oxaliplatin, that has been used clinically for the treatment of a variety of solid tumors.

Metallic Nanoparticles



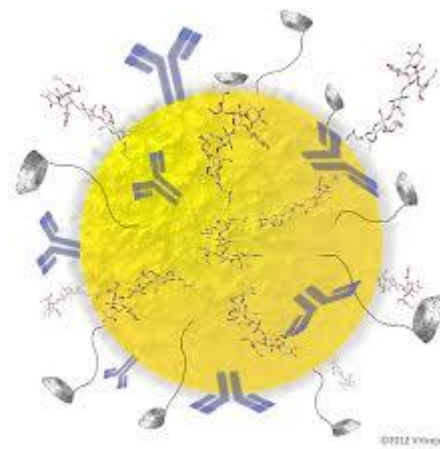
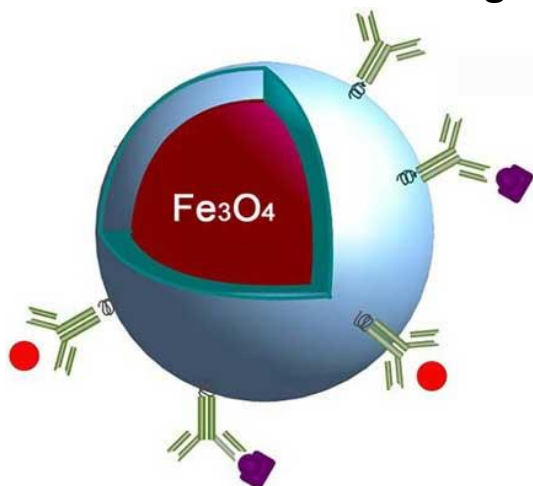
Metallic nanoparticles have unique characteristics such as magnetic and optical properties

targeted drug delivery

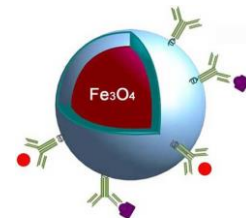
diagnostic imaging

THERANOSTIC AGENT

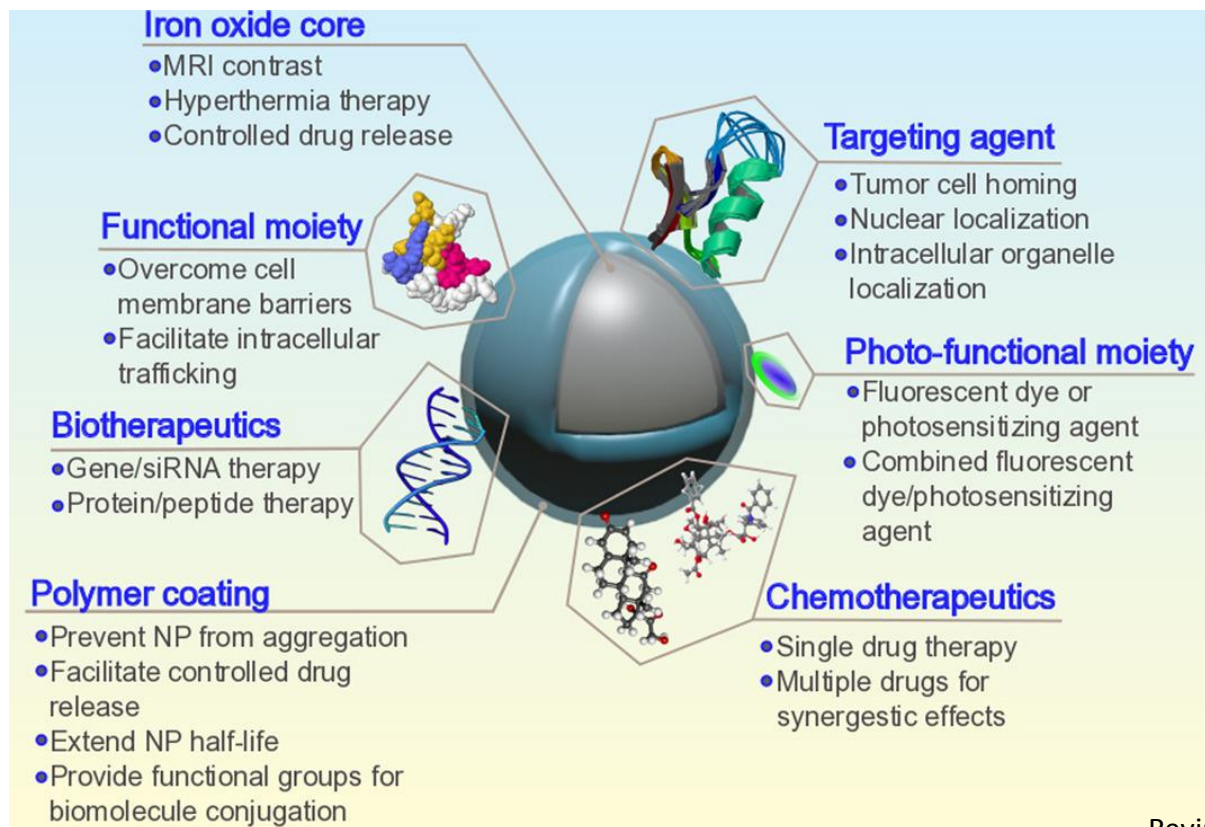
magnetic (Fe_3O_4) and gold nanoparticle



Magnetic nanoparticles (MNP)



Current Drug Metabolism,
Volume 17 , Issue 8 , 2016

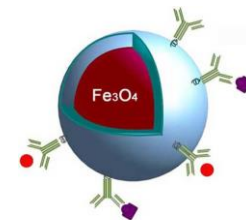


Revia RA et al. Materials Today
Volume 19,Number 3 April 2016

The most frequently used nanomaterial is the iron oxide nanoparticle, including magnetite (Fe_3O_4) and maghemite ($\gamma\text{-Fe}_2\text{O}_3$).

MNPs are generally in the superparamagnetic state ($< 20 \text{ nm}$) (SPION)

MNP: synthesis methods



Current Drug Metabolism,
Volume 17 , Issue 8 , 2016

SPION are synthesized using a wide range of methods

Coprecipitation does not allow for good control of particle geometry and size distribution.

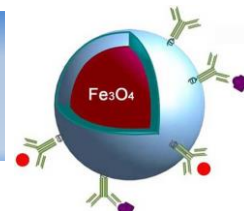
thermal decomposition in the oil phase can produce high-quality hydrophobic iron oxide NPs with perfect monodispersity and high crystallinity

microemulsion technique has the advantage of controlling the size of NPs by acting as a nanoreactor.

hydrolysis method and microwave-assisted synthesis produce NPs showing good water dispersibility and low cytotoxicity in the way of hydrolysis

Two main surface-modification strategies are able to improve the water dispersibility of SPION: (i) a ligand exchange process in order to replace original hydrophobic ligands and (ii) surface encapsulation with amphiphilic polymers

MNP: applications



Current Drug Metabolism,
Volume 17 , Issue 8 , 2016

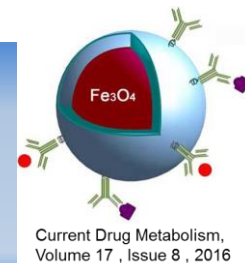
Formulations of SPIONS already gained approval by the Food and Drug administration (FDA) in clinic as:

- ✓ **iron deficiency therapeutics (Feraheme)**
- ✓ **as MRI contrast agents(Gastromark)**

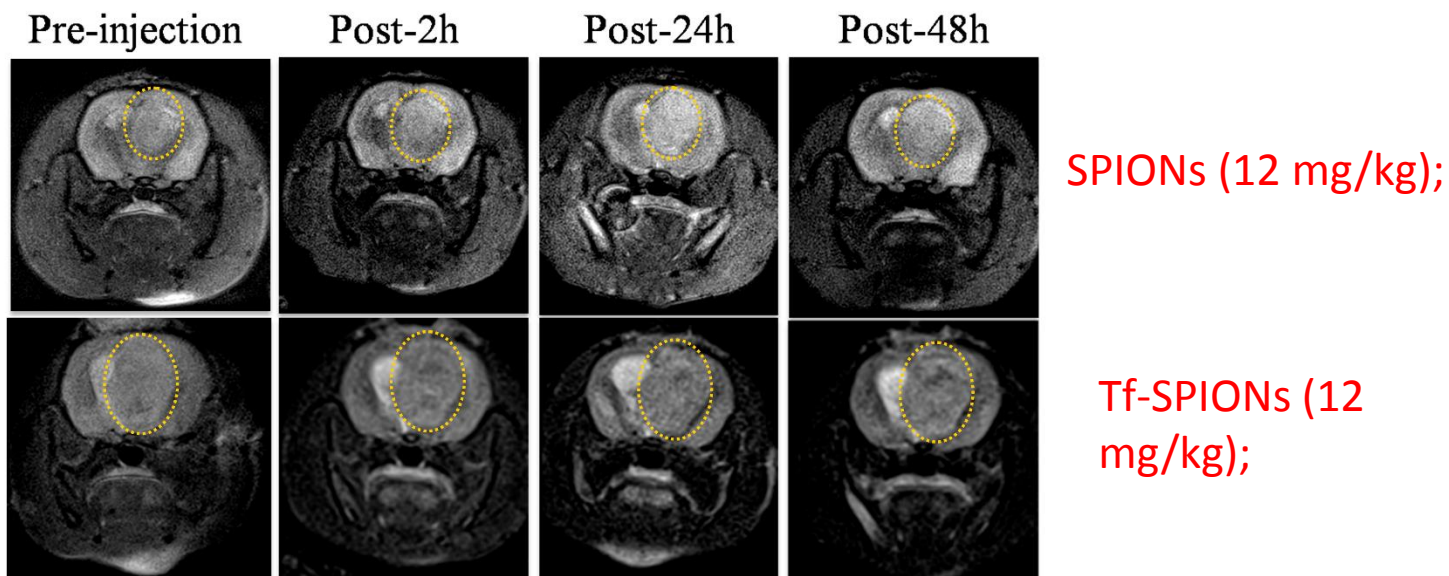
Development of the MNP also for:

- ✓ **Targeted MRI contrast agents**
- ✓ **Multimodal imaging**
- ✓ **Therapeutic treatment**
- ✓ **Monitoring cancer treatment in an efficient and effective manner**
- ✓ **Theranostic platforms**

SPIOs for targeted MRI imaging



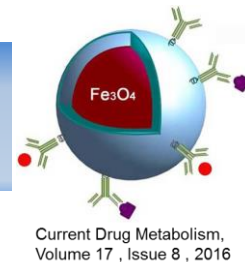
Transferrin-conjugated superparamagnetic iron oxide nanoparticles (Tf-SPIONs), in rat brain glioma models.



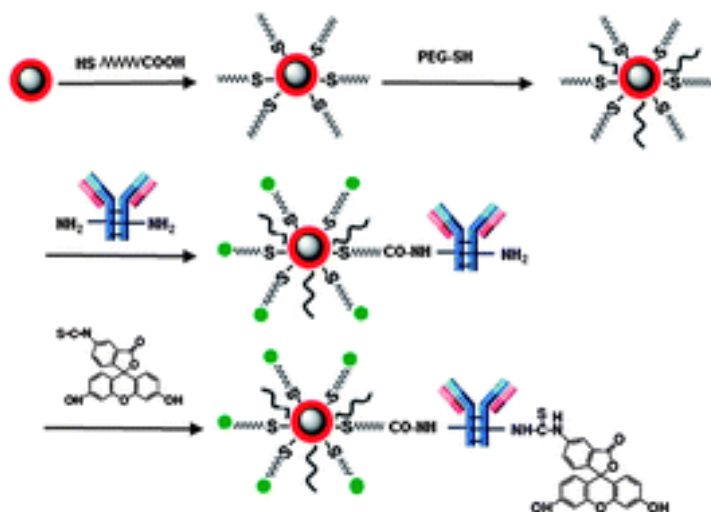
Jiang W et al., PlosOne 2012, 5 , e37376

The changing area of decreased MR signal intensity increased gradually with timing up to 48 h in comparison to the preinjection image of tumor.

MNP: Multimodal imaging



Multifunctional probe for targeting avb3 integrin and multimodal imaging of cancer cells simultaneously.



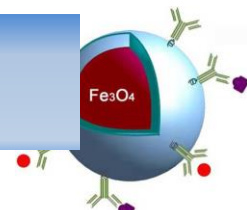
J. Mater. Chem., 2012, 22, 470

core-shell Fe₃O₄@Au NPs

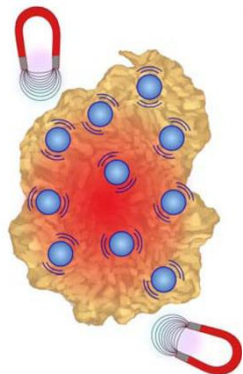
With the Fe₃O₄@Au NPs, we can identify the specific location of tumor in the body before surgery with a MRI, and then use fluorescence imaging to find and remove all parts of the tumor during the operation

SPION when conjugated with a fluorescent dye, they can also be used for fluorescence imaging, which has a much higher sensitivity than the MRI imaging

MNP: magnetic hyperthermia



Current Drug Metabolism,
Volume 17 , Issue 8 , 2016



The innate magnetic properties of SPIONs may be harnessed to provide localized hyperthermia that induces tumor necrosis by applying an external magnetic field making SPIONs therapeutic without the addition of functional moieties

Revia RA et al. Materials Today Volume
19, Number 3 April 2016

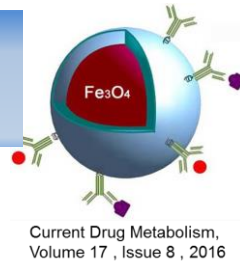
Magnetic Hyperthermia



Therapeutic effect

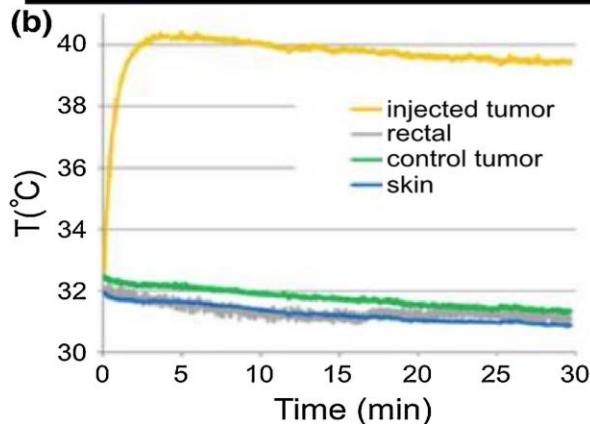
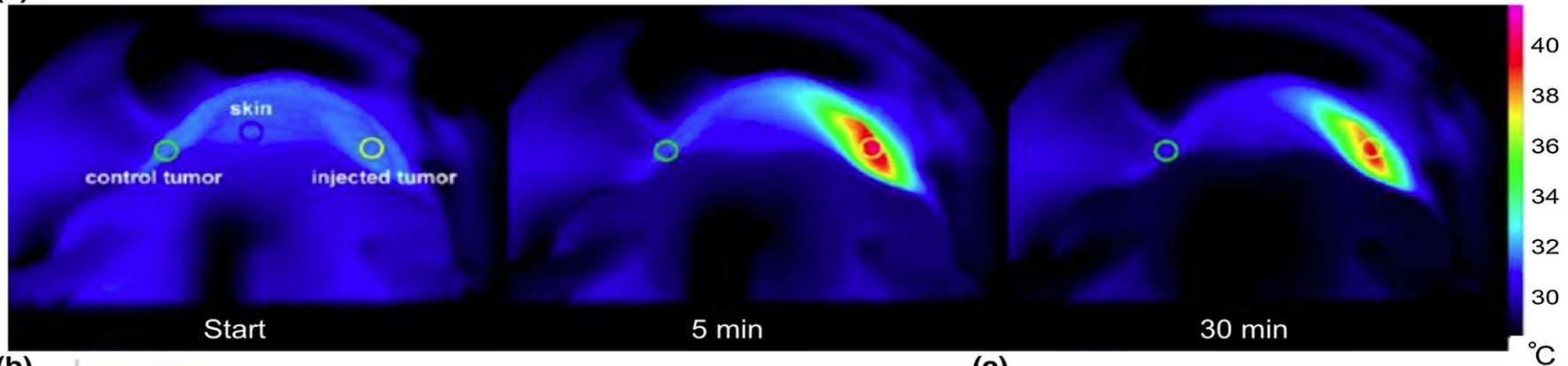
Drug releasing trigger

MNP: magnetic hyperthermia

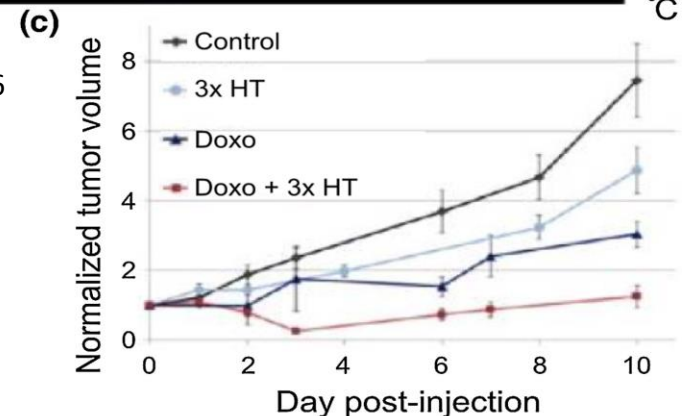


PEG-coated magnetite NPs were able to reduce tumor growth through magnetic hyperthermia when intratumorally injected into epidermoid carcinoma xenograft implanted mice

(a) *thermographic infrared photographs taken at different timepoints during magnetitc hyperthermia*



Revia RA et al. Materials Today
Volume 19, Number 3 April 2016



profiles of various organ systems during the magnetic hyperthermia therapy; off-site temperature levels retained normal values whereas the tumor tissue experienced elevated temperatures.

the destruction of the extracellular matrix caused by magnetic hyperthermia led to increased drug penetration

MNPs: Drug release trigger

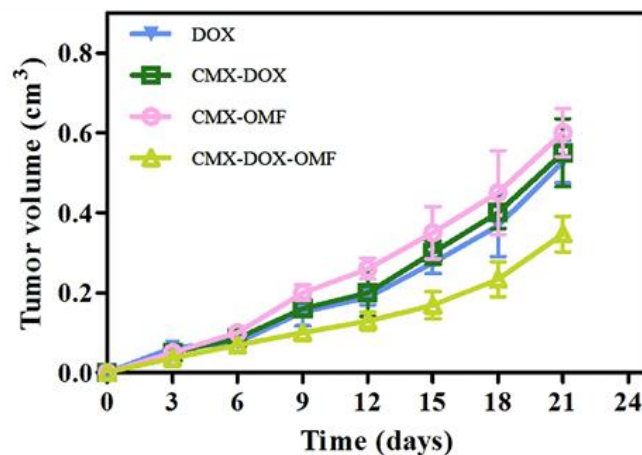


Magnetite NP coated with carboxymethyldextran and loaded with doxorubicin

(A)



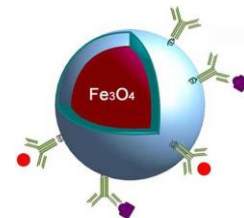
Magnetic hyperthermia effect can be also used as a drug-releasing trigger. If drugs are encapsulated in a heat labile coating, then controlled release of drugs may be achieved with magnetite NPs when they heat up due to the application of an external magnetic field.



changes in tumor volume over 21 days

Hua X, Drug Deliv, 2017;
24(1): 511–518

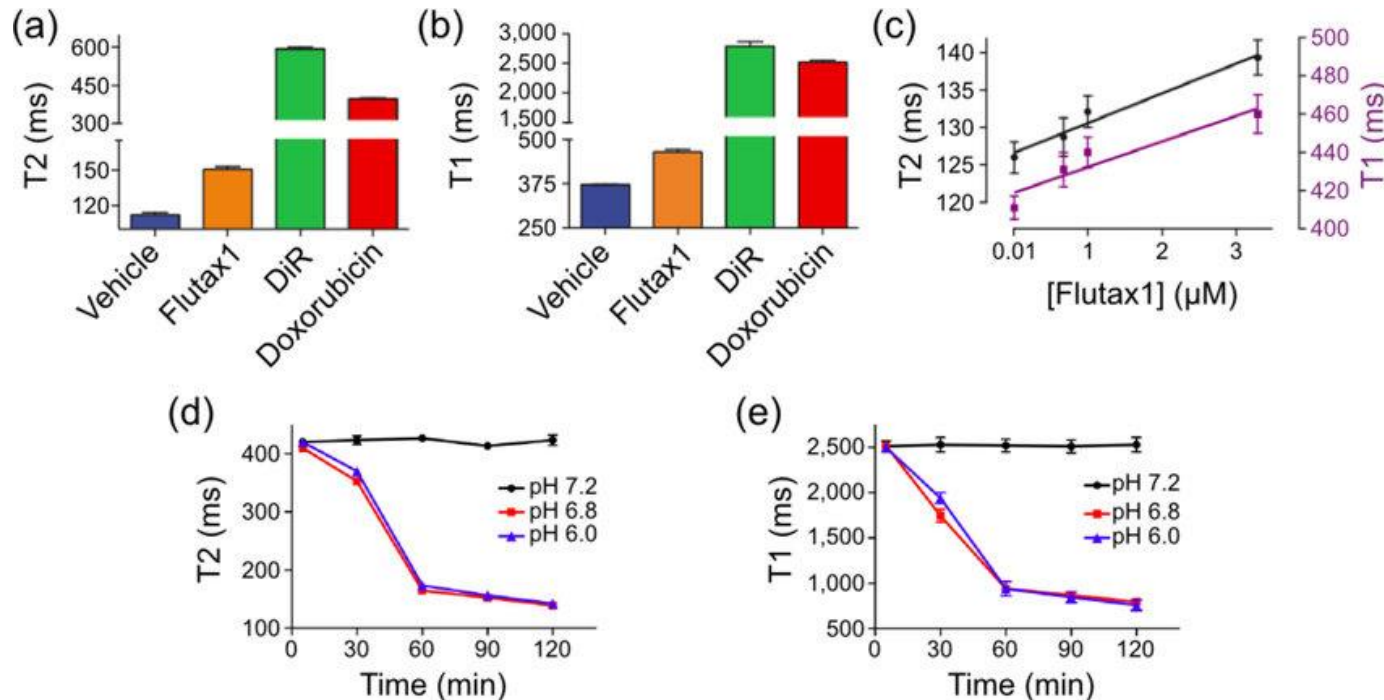
MNP: monitoring treatment



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Volume 17, Issue 8, 2016

Drugs loaded onto iron oxide NPs and then coated in a pH sensitive polymeric coating

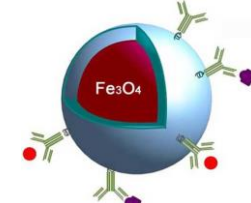
Drugs loaded onto NPs may hinder water's access to NP cores and thereby nullifies their ability to alter the relaxation times of protons



Revia R.A et
al. Materials
Today
19, Number 3
April 2016

Doxorubicin loaded NPs released the drug when exposed to pH environments of 6.8 or less, and drug release consequently reduced the T1 and T2 values of the NPs. This demonstrates how MRI may be used to monitor cargo release from iron oxide NPs.

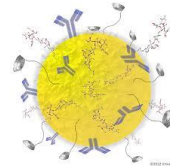
Metallic NPs in imaging and therapy



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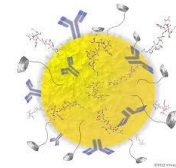
| NP Core Composition | NP Coating | Hydrodynamic size | Loaded Drug | Targeting Ligand | Cell/In Vivo Model | Application | Ref |
|------------------------------|------------------|-------------------|--|---|--|---|-----|
| Bismuth-iron oxide composite | Dextran | 98 nm | None | None | Human liver carcinoma cells (Hep G2) BJ5ta fibroblasts C57BL/6J mice | Dual CT and MRI T2 contrast agents were successfully deployed in an in vivo murine model | 41 |
| Iron oxide | PEG | 10 nm | None | None | J774 macrophages | SPIONs capable of enhancing T1 contrast in MRI were developed and tested in vivo | 45 |
| Iron oxide | None | 35 nm | None | Anti-prostate specific membrane antigen J591 antibody | LNCaP cells (CRL-1740) DUI145 cells (HTB-81) | MRI T2 contrast agents that specifically target prostate cancer cells were developed | 48 |
| 18F-iron oxide | Dextran | 30 nm | None | None | BALB/c mice | Trimodal imaging contrast agents providing MRI, PET, and CT capabilities were evaluated in vivo | 59 |
| Iron oxide | Dextran | 40 nm | Flutax1 DiR Doxorubicin | None | LNCaP cells Mice with PC3 flank xenografts Mice with BT20 flank xenografts | Drug delivery vehicles that release their therapeutics in mildly acidic environments were created; these particles also exhibit changes in MR relaxivity values upon drug release and may thus be used to monitor drug delivery | 66 |
| Iron oxide | Chitosan | 50 nm | Temozolomide | Chlorotoxin | Glioblastoma cells (U-118 MG) C57BL/6J mice | Drug delivery vehicles capable of carrying the chemotherapeutic temozolomide specifically to glioblastoma brain cancer cells were tested in vitro | 70 |
| Iron oxide | PEI | 100 nm | siRNA targeting human telomerase reverse transcriptase | None | MCF-7 cells PC3 cells SKOV-3 cells Hep G2 cells BALB/c mice with Hep G2 xenograft tumors | Redox-sensitive gene and siRNA delivery was achieved in vitro and in vivo to induce apoptosis and inhibit growth of liver cancer | 77 |
| Iron oxide | Chitosan PEG PEI | 40 nm | Apurinic endonuclease 1 suppressing siRNA | None | Medulloblastoma cells (UW228-1) Ependymoma cells (Res196) | In vitro delivery of siRNA to two types of brain tumor cells was facilitated by iron oxide NPs; the siRNA reduced the activity of an enzyme implicated in radiation resistance in tumors | 79 |
| Iron oxide | PEG | 19 nm | None | None | Immunodeficient athymic NMRI mice Human epidermoid carcinoma xenografts (A431 cells) | SPIONs injected intratumorally into skin cancer xenografts induced localized hyperthermia when irradiated with an external magnetic field, arresting tumor growth | 83 |
| Iron oxide | PEG | 75 - 200 nm | Doxorubicin Paclitaxel | IVO24 peptide | Human cervical carcinoma cells (HeLa) Human breast carcinoma cells (MCF-7) Mice bearing MCF-7 tumors | Dual-drug loaded, therapeutic delivery vehicles that release drugs upon exposure to an external magnetic field were used to treat breast and cervical cancer models in vitro and in vivo | 84 |
| Gold-iron oxide composite | PEG | 25 nm | None | A33 scFv antibody | Colorectal cancer cells (SW1222 and HT 29) | Active targeting of colorectal cancer cells and subsequent selective photothermal ablation of tumor tissue in vivo | 88 |
| Iron oxide | APTES | 15 nm | Pheophorbide-A | None | Epithelial cancer cells (KB cells) | Simultaneous photodynamic therapy and dual-mode fluorescence/MR imaging of epithelial cancer cells in vitro was demonstrated | 94 |
| Iron oxide | PEG | 100 nm | Chlorin e6 | None | Murine breast cancer cells (4T1) BALB/c mice | In vitro and in vivo photodynamic therapy was used to treat breast cancer in a murine model; cancer tissue was specifically targeted by drawing NPs to tumor sites via an external magnetic field | 95 |

Gold nanoparticle (AuNP)



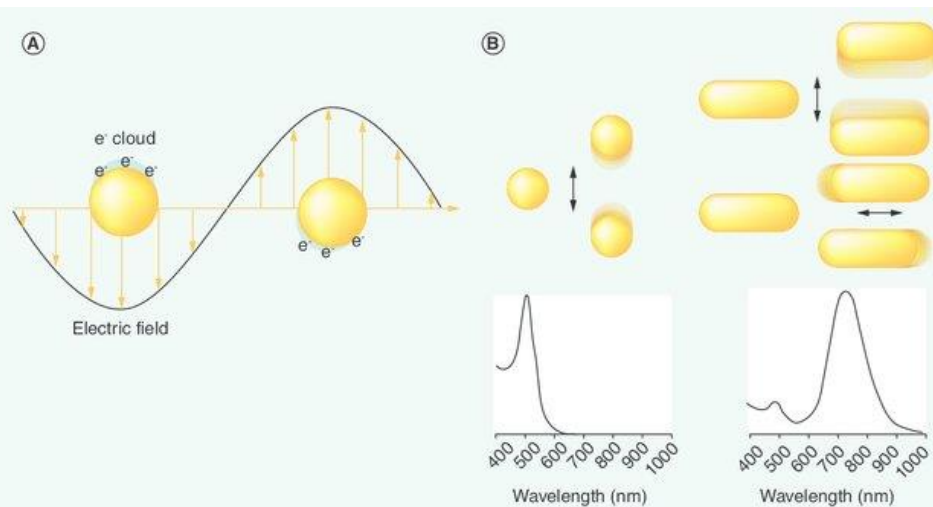
- ❖ Medicinal application of gold and its complexes also has a long history.
- ❖ The first data on colloidal gold (colloidal suspension of nanoparticles of gold in a fluid) can be found in ancient Chinese, Arabian, and Indian papers from V–IV centuries BC, which recommended it for the treatment of various diseases, although the mechanism of action was poorly understood. In medieval Europe, colloidal gold was frequently studied in alchemist laboratories and used for the treatment of mental diseases, syphilis, diarrhea, and even recommended as the elixir of longevity.
- ❖ In the last 40 years several studies are devoted to biomedical applications of gold nanoparticles

AuNP : optical properties



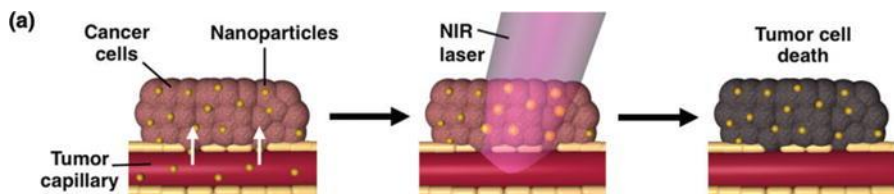
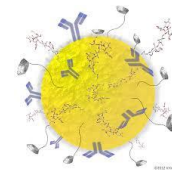
Surface plasmon resonance (SPR) a phenomenon occurs when the frequency of the oscillation of free conductive electrons at the surface of the nanoparticle resonates with the frequency of the incoming light radiation, resulting in a plasmon band.

(A) The electromagnetic field of incident light induces coherent collective oscillation of conduction band electrons. (B) Comparison between nanospheres and nanorods, showing that the dipolar oscillation depends on particle size and shape. While nanospheres show one surface plasmon resonance band, nanorods have two: a strong longitudinal band in near-infrared region (long axis) and a weak transverse band (short axis).





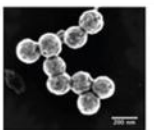
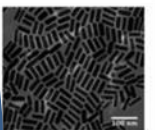
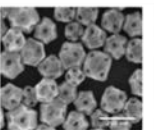
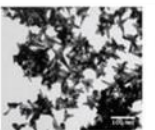


AuNPs provide both absorption and scattering effects, depending on the size and shape but also on the type of solvent, surface ligand, core charge, temperature, and the proximity of other nanoparticles, influencing the electron charge density on the particle surface

AuNP : Photothermal therapy



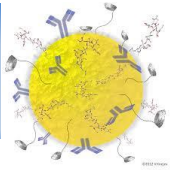
(b)

| | Nanoshells | Nanorods | Nanocages | Nanostars |
|----------------------|---|---|---|---|
| Schematic |  |  |  |  |
| SEM |  |  |  |  |
| Size for PTT | ~150 nm diameter | ~10 nm x 40 nm | ~40-60 nm length | ~45-120 nm |
| Stage of development | Clinical trials: lung, head & neck, and prostate cancer | Preclinical | Preclinical | Preclinical |
| Unique features | Core:shell structure | Two resonance peaks | Drug loading capabilities | Large surface area for bioconjugation |

- ✓ The irradiation in the range of SPR is followed by rapid conversion of light into heat that causes the disruption of cellular membranes and protein denaturation leading to cell death.
- ✓ The damage on the healthy tissue can be partially overcome by the use of laser radiation enabling the controlled and precise destruction of cancer tissue.
- ✓ Size, shape, and structure greatly influence photothermal properties
- ✓ Near infrared (NIR) light is chosen for PTT due to minimal absorption by the tissues at these wavelengths (650–900 nm)

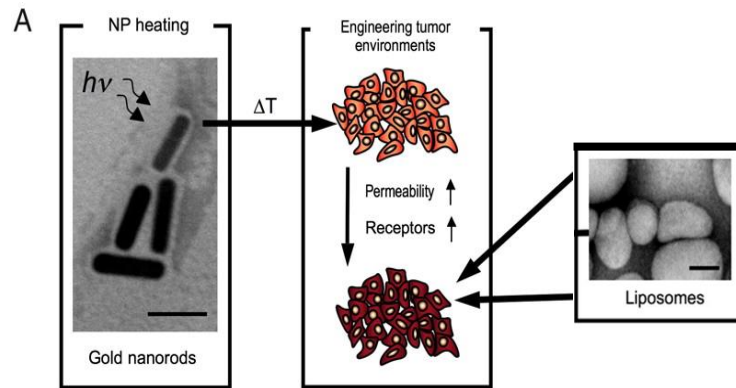
➤ Nanoshells coated with PEG (AuroLase, commercialized by Nanospectra Biosciences, Inc.) are currently the only AuNP for PTT being evaluated in clinical trials

AuNP : Photothermal therapy

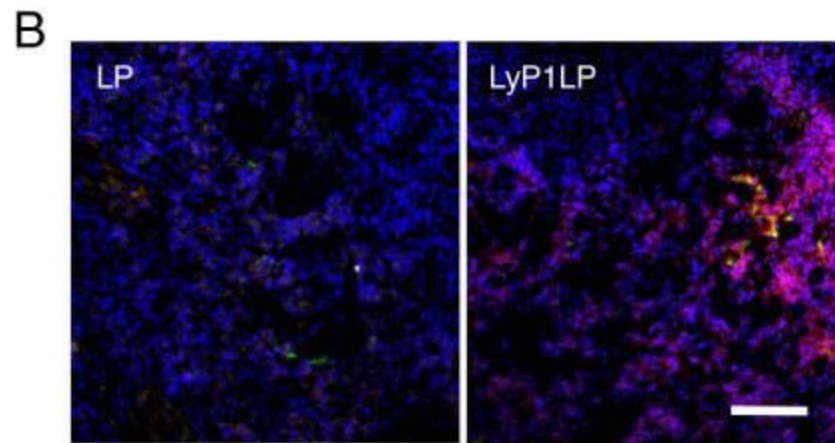
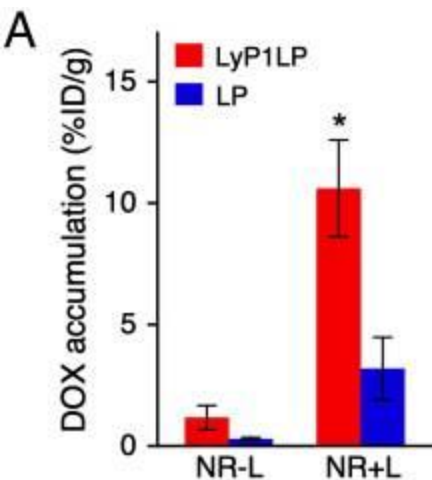


Cooperative nanosystem in mice bearing MDA-MB-435 tumors

Dox-loaded liposomes + AuNR



A cooperative system that targeted drug-loaded liposomes to the p32 protein, which is upregulated following NR mediated PTT, to improve tumor delivery of the drugs and enhance treatment outcome versus PTT or chemotherapy individually has been prepared.

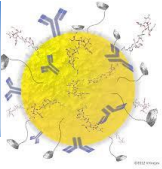


Amount of DOX present was quantified by fluorescence microscopy to yield a percentage of injected dose per tissue mass. (B)

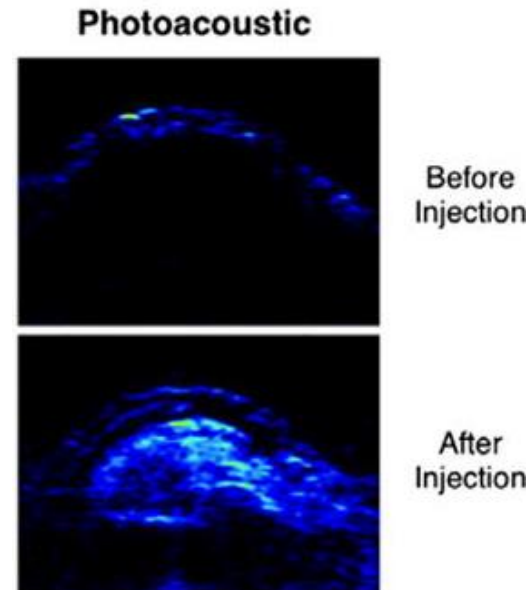
Histological analysis of DOX (Alexa Fluor® 488 label on control liposome and 5(6)-carboxyfluorescein (FAM) label on LyP-1, Green) and DOX (Red)

LyP-1-conjugated liposomes
Non conjugated liposomes

AuNP : Photoacoustic imaging



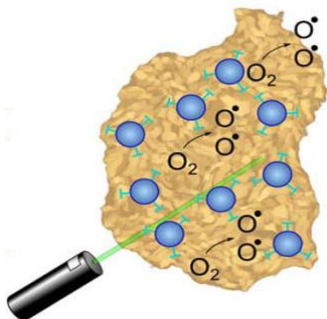
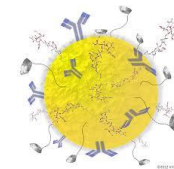
In PA imaging, tissue is irradiated with a pulsed laser and light absorption produces a temperature rise in the tissue leading to its subsequent thermo-elastic expansion. The pressure induced by this expansion leads to propagation of acoustic waves, which are detected by an ultrasound transducer at the surface of the body



WIREs Nanomed
Nanobiotechnol 2017,
9:e1449

photoacoustic images demonstrate enhanced signal from biodegradable gold-based NPs accumulated within the tumor. NPs were composed of clusters of small gold nanoparticles that produced an ultrastrong plasmonic coupling effect for imaging and PTT.

AuNP : Photodynamic therapy



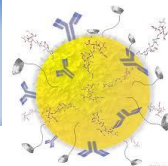
Metal nanoparticles find application as photosensitizers in photodynamic therapy (PDT). It is an alternative cancer treatment modality, which, in principle, is far more effective than PTT, where every singlet O_2 molecule can facilitate the destruction of cancer cells, and, unlike PTT effect, will not be suppressed by low temperatures

Vankayala R.,
Biomaterials 2014, 35,
5527-5538

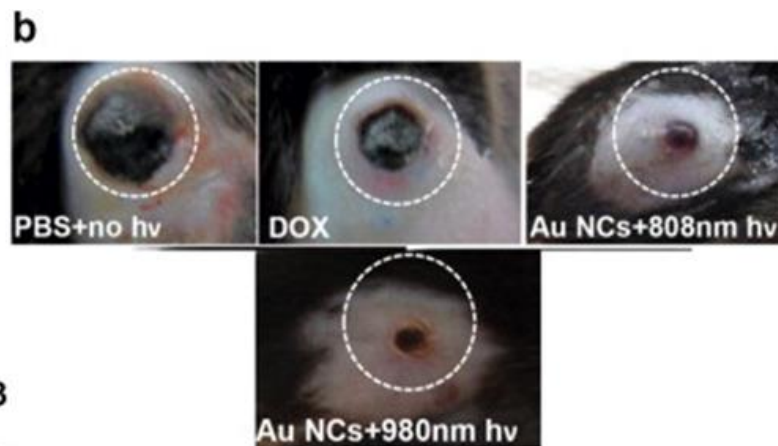
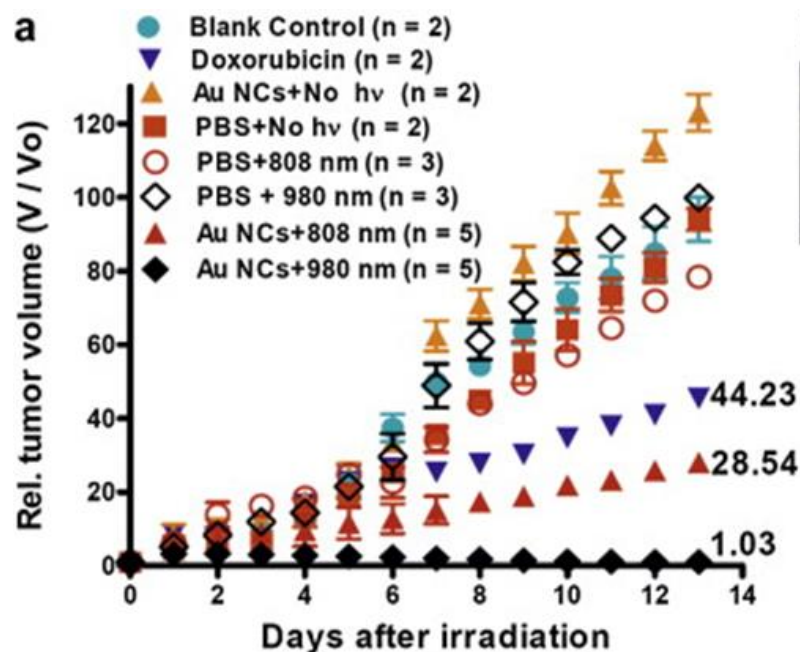
Most of the organic photosensitizers used in clinical PDT treatments are, however, restricted to be activated only by UV and visible light, which has very poor tissue penetration depths and therefore limited to the treatments of surface tumors

In metal nanostructures thank to their SPR effect upon photoexcitation, the excited state photon energy can undergo energy transfer to molecular oxygen and generate highly reactive oxygen species, such as singlet oxygen.

AuNP : Photodynamic therapy



Multimodal systems : PTT and PDT effect



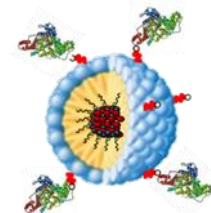
Vankayala R.,
Biomaterials 2014, 35,
5527-5538

In vivo phototherapeutic effects from Au nanocages in B16F0 melanoma implanted mice.

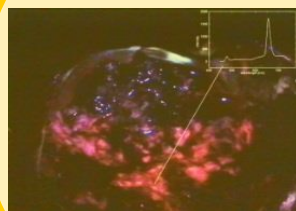
(a) Tumor growth curves of different groups of tumor-bearing mice after treatment. The tumor volumes were normalized to the initial sizes.

b) Representative images of mice showing the sizes of tumors at day 14 after treatment for PBS-injected mice without light, doxorubicin injected mice and lipid-coated Au nanocages injected mice after exposure to 808 and 980 nm laser wavelengths respectively.

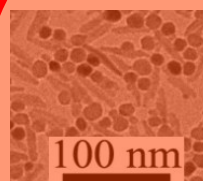
Binary Nanocrystalline Heterostructures (BNC)



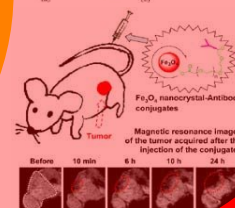
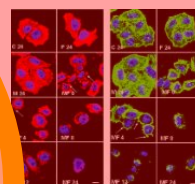
Photodynamic
therapy



TiO_2 domain



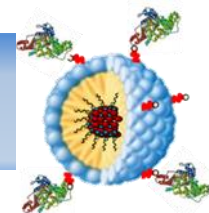
Hyperthermia



In vivo Imaging

Fe_2O_3 domain

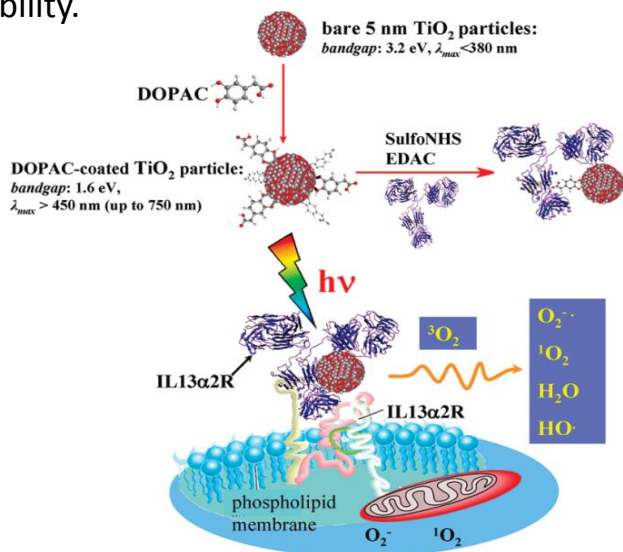
BNC: multimodal properties



TiO₂

It is among the promising photosensitizer for photodynamic therapy (PDT) against cancer

Semiconductor characterized by excellent photocatalytic activity, low toxicity and high chemical stability.



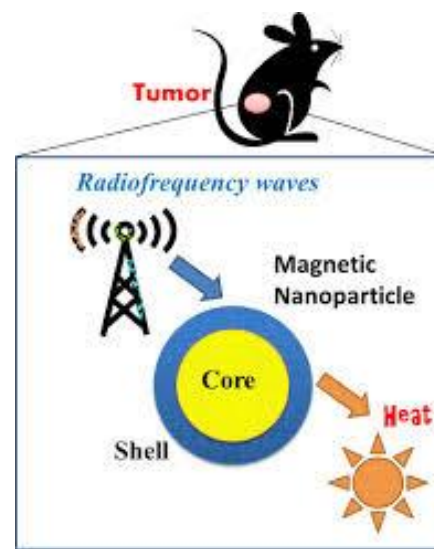
PDT is a form of phototherapy where light-sensitive compounds (photosensitizers), exposed selectively to light, leads to the formation of powerful oxidative radicals able to destroy the tumor cells.

UV-light is brought into the tumour site using an UV-fiber. Using an on – operation MRI technique the real –time MRI and in situ PDT could be realized

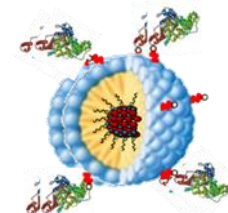
γ-Fe₂O₃

Superparamagnetic iron oxide NPs show a superior biocompatibility and a greater sensitivity in the micromolar or nanomolar range than other agents, such as gadolinium complexes, in MRI.

Magnetic nanoparticles induce hyperthermia when subjected to an alternating magnetic field of suitable amplitude and frequency.

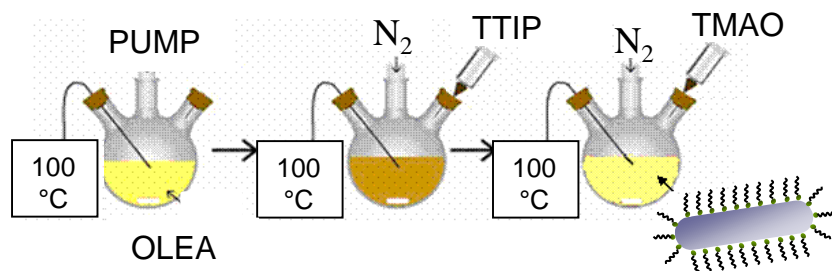


BNC: synthesis

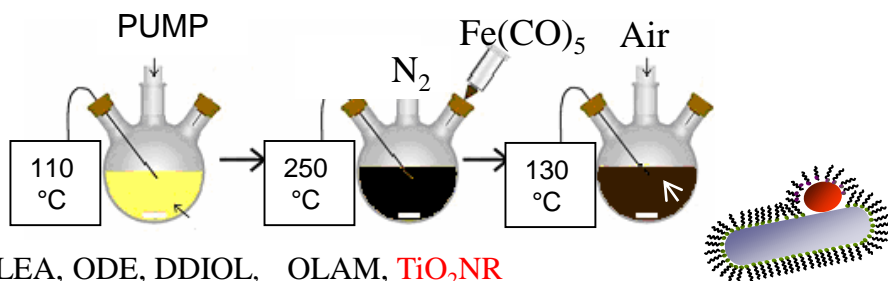


Colloidal chemical approach

1. TiO₂ Nanorods (NRs)



2. TiO₂ - γ-Fe₂O₃ Heterostructures (BNCs)

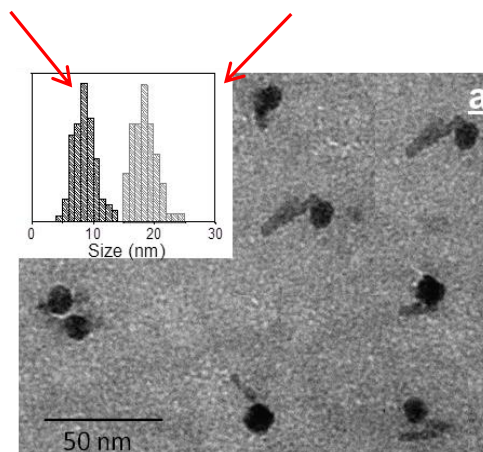


OLEA, ODE, DDIOL, OLAM, TiO₂NR

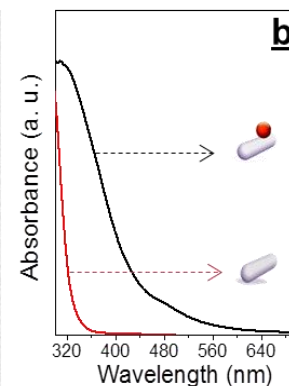
TTIP Titanium Tetraisopropoxide, Fe(CO)₅ Iron Pentacarbonyl, ODE 1-Octadecene, OLAM Oleylamine, DDIOL Dodecan-1,2-Diol, TMAO Trimethylamino-N-Oxide, OLEA Oleic Acid

Fe₂O₃ NDs (8nm, σ%=15)

TiO₂ NRs (18nm, σ%=10%)

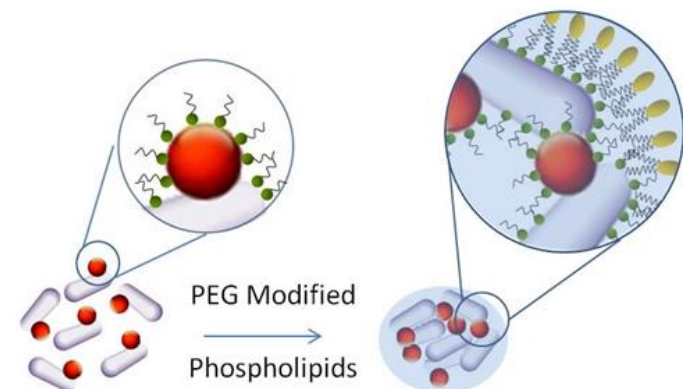
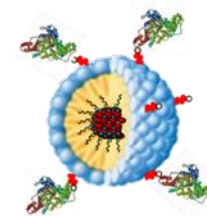


TEM micrograph of organic capped BNCs cast from chloroform (a) Particle size distribution of (gray) TiO₂ NRs and (black) Fe₂O₃ NCs (inset a) NCs.

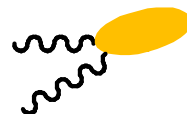


Absorption spectra of organic capped pure TiO₂ NRs and BNCs Enhancement of visible light absorbance

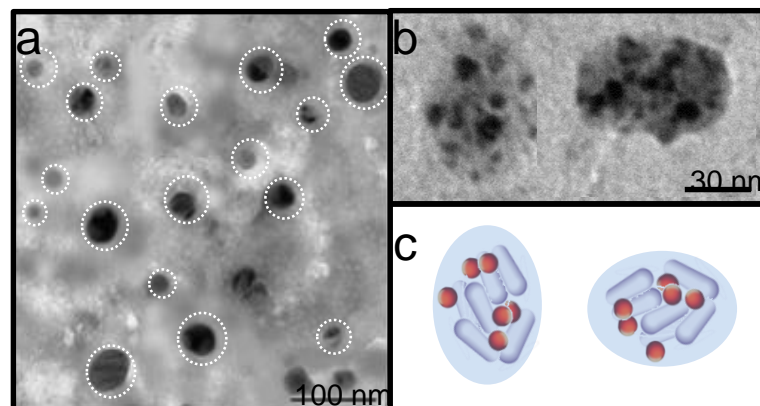
BNC: encapsulation in PEG micelle



Surfactant capped BNC

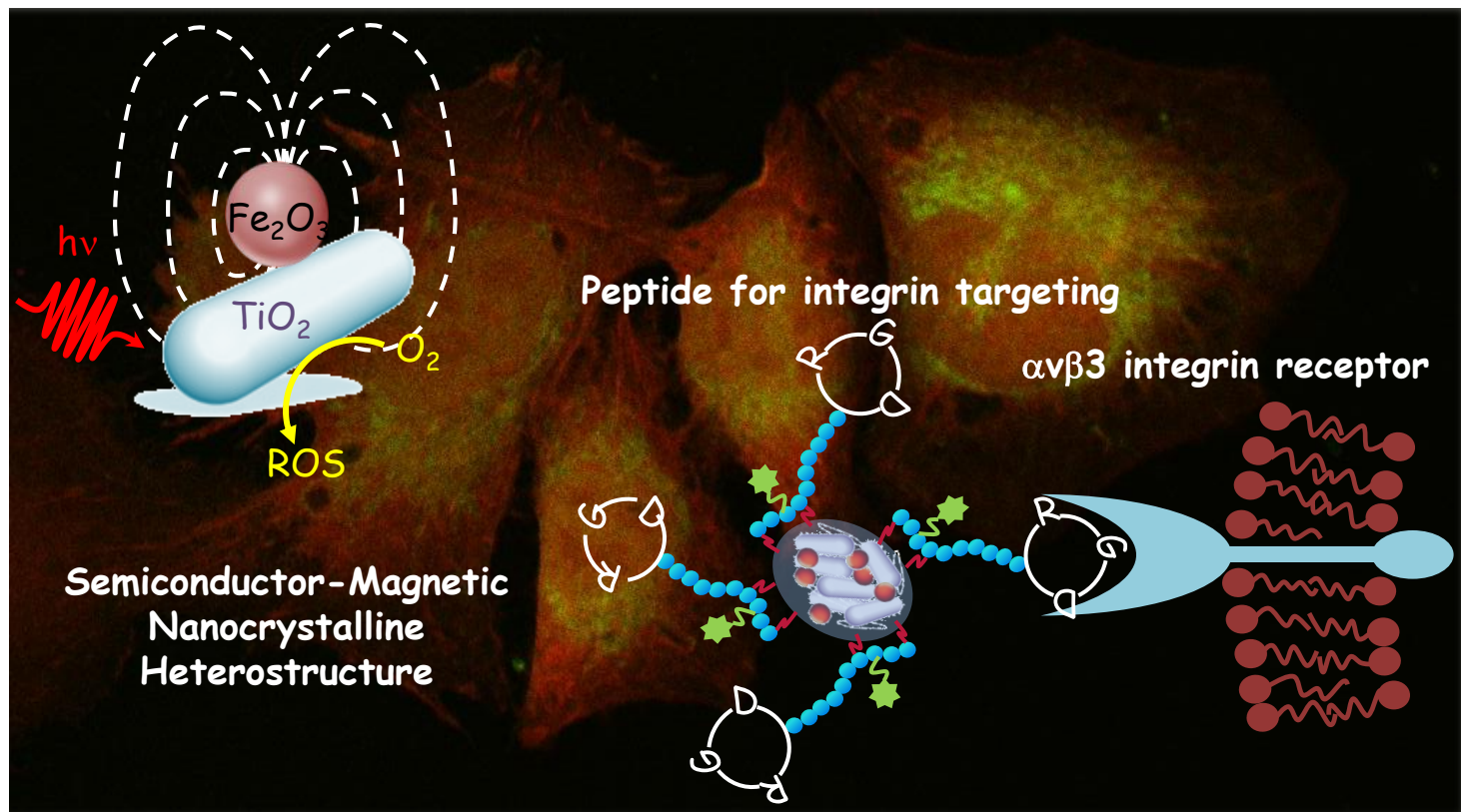
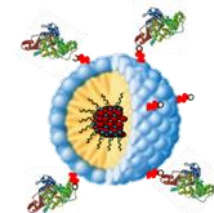


(1,2-Dipalmitoyl-*sn*-Glycero-3-Phosphoethanolamine-N-[Methoxy(PolyethyleneGlycol)-2000]
(PEG-PE) (3.5×10^{-2} M)
1,2-Distearoyl-*sn*-Glycero-3-Phosphoethanolamine-N-[Carboxy(PolyethyleneGlycol)2000]
(DSPE-PEG-COOH) (3.5×10^{-2} M)

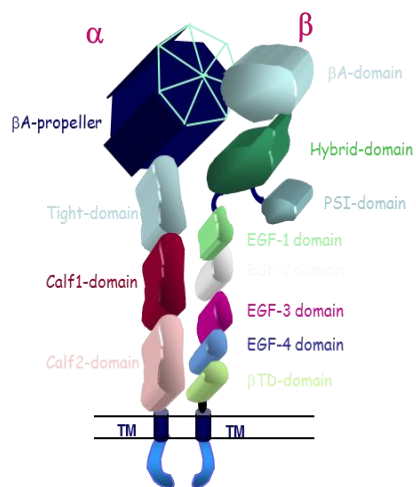


TEM micrographs with positive (a) and negative (b) staining of BNC/Micelles clearly indicates that the micelle diameter ranges from 15 to 70 nm, indicating the formation of aggregates in a wide range of sizes, containing a variable number of BNCs clustered in a single micelle.

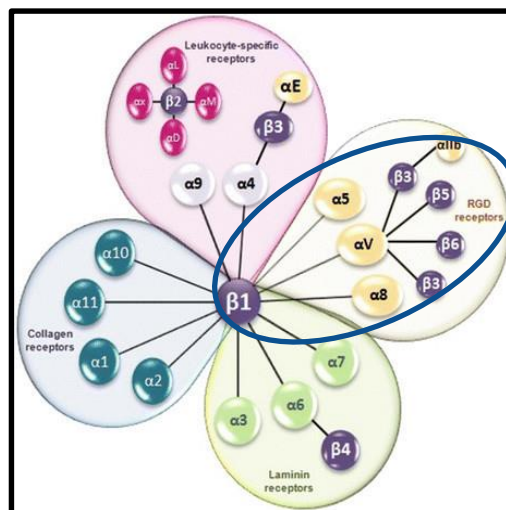
BNC: active targeting



Valente G., Depalo N., de Paola I., Iacobazzi R. M., Denora N., Laquintana V., Comparelli R., Altamura E., Latronico T., Altomare M., Fanizza E., Striccoli M., Agostiano A., Saviano M., Del Gatto A., Zaccaro L*. and Curri M. L.*, Nanoresearch, 2016, 644-662.



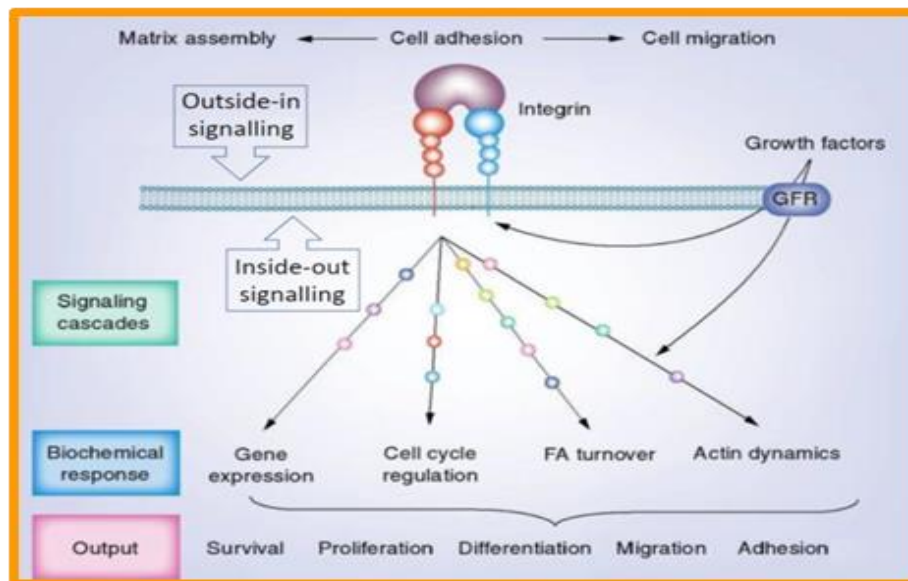
Intracellular environment



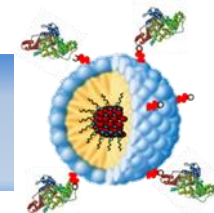
Glioma cell Biology: Chapter 4





Arg-Gly-Asp
receptors

✓ 24 subtype integrins derived by the combination of the different α and β -subunits.

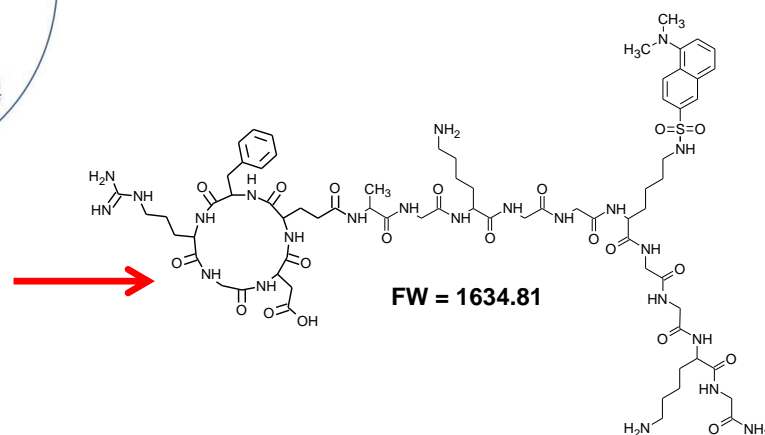
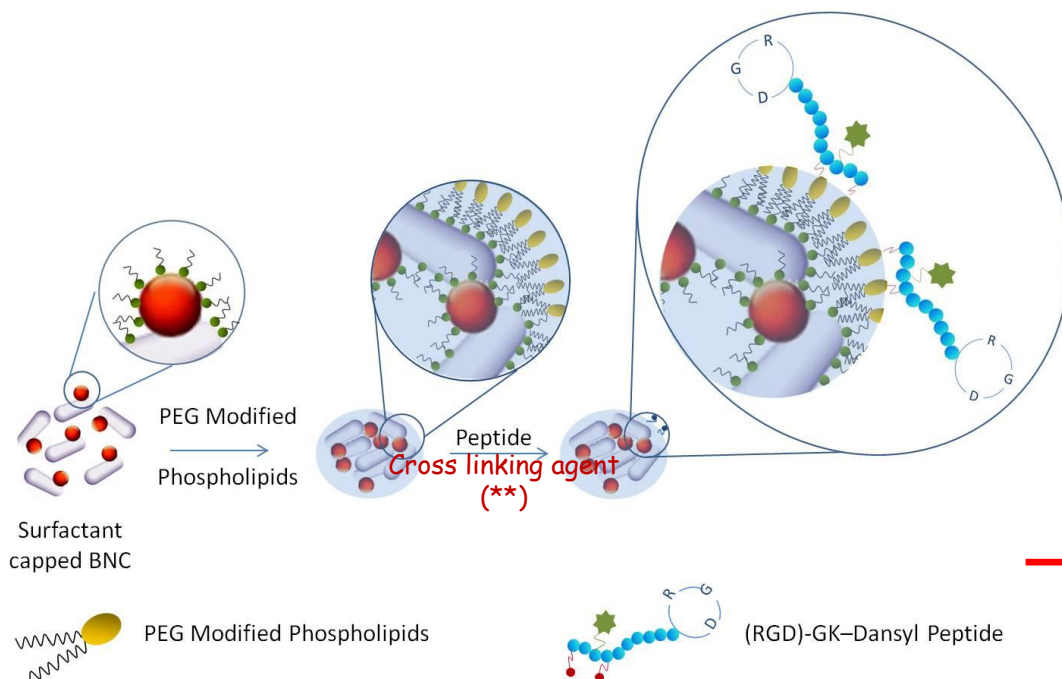
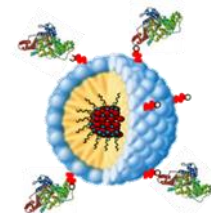


$\alpha v \beta 3$ integrin as tumor marker

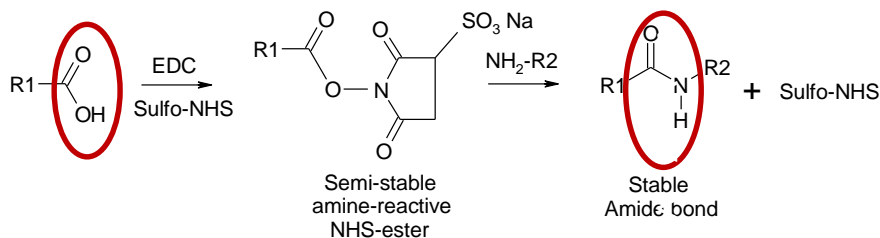


-  highly expressed on activated endothelial cells and new-born vessels in tumors, but it is completely absent in the rest of endothelial cells and in most normal organs.
-  Its high expression is correlated with tumor invasion and poor prognosis in melanomas, glioma, prostate and breast cancer
-  $\alpha v \beta 3$ integrin is a marker of cancer stem cells and is associated with epithelial-to-mesenchymal transition
-  It is involved in the transformation of drug resistance and tumor recurrence

BNC/Micelle: bioconjugation

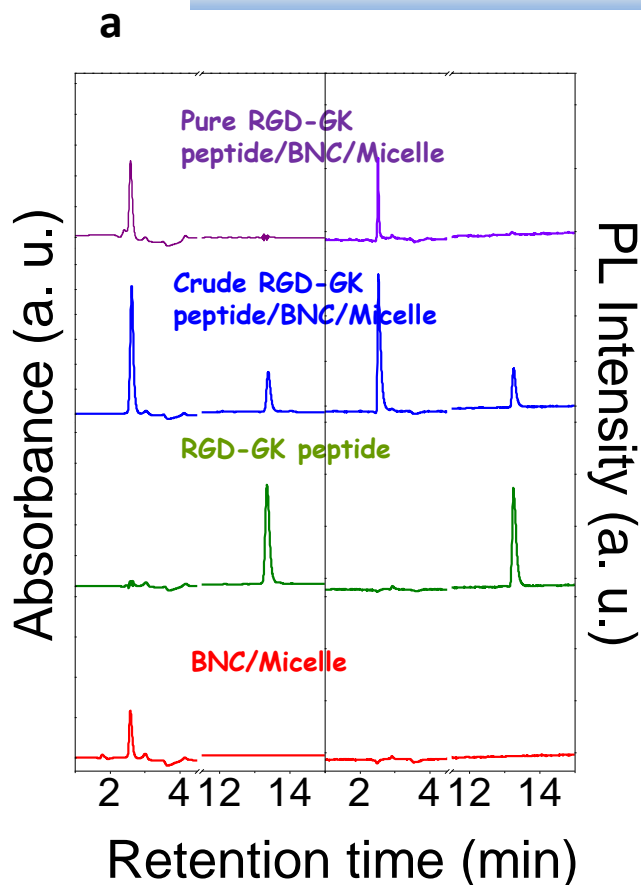
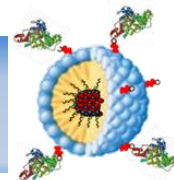


Scheme. EDC/Sulfo-NHS Conjugation Reaction



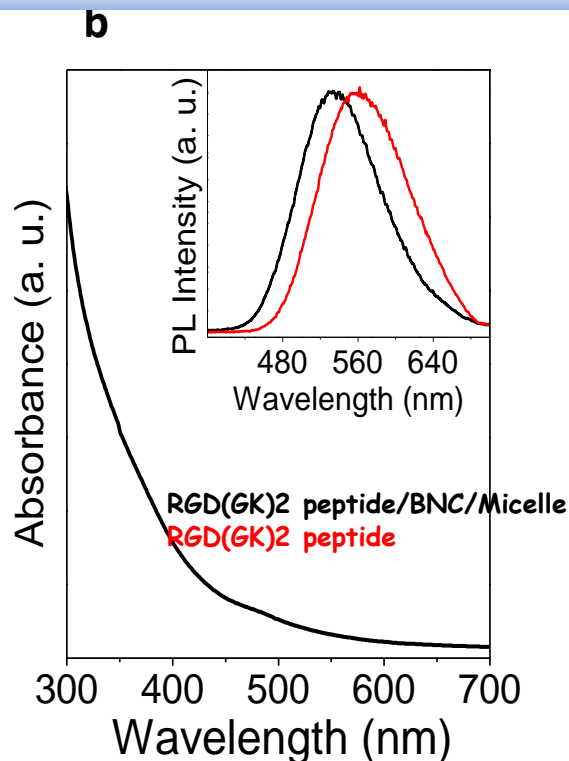
| [COOH] (M) | [EDQ] (M) | [SulfoNHS] (M) | [(GK)2DNS Peptide] (M) | t _{reaction} (hr) |
|--------------------|--------------------|-----------------------|---------------------------|-------------------------------|
| 5.10 ⁻⁴ | 5.10 ⁻³ | 1.25.10 ⁻² | 1.0.10 ⁻⁴ | 2 |
| 5.10 ⁻⁴ | 5.10 ⁻³ | 1.25.10 ⁻² | 1.5.10 ⁻⁴ | 2 |
| 5.10 ⁻⁴ | 5.10 ⁻³ | 1.25.10 ⁻² | 5.0.10 ⁻⁴ | 2 |
| 5.10 ⁻⁴ | 5.10 ⁻³ | 1.25.10 ⁻² | 1.10 ⁻³ | 2 |

(**) 1-Ethyl-3(3-Dimethylaminopropyl)Carbodiimide Hydrochloride (EDC), N-Hydroxysulfosuccinimide (Sulfo-NHS)

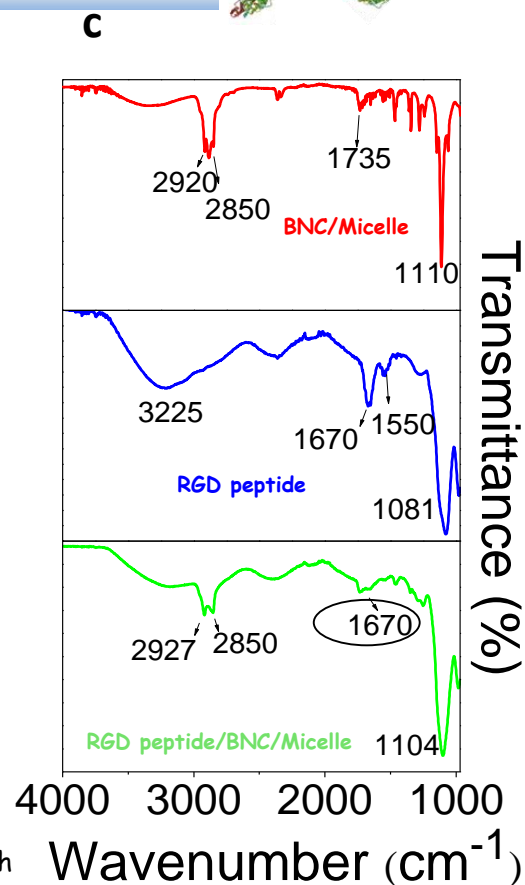


The efficiency of purification has been investigated by means of HPLC analysis, using UV-Vis and fluorescence detectors. The PL signals has been recorded at 560 nm ($\lambda_{ex} = 329$ nm)

[RGD(GK)2-peptide] conjugated to BNC/micelle surface has been estimated, by PL measurements, to be 98 ± 4 $\mu\text{g/mL}$,



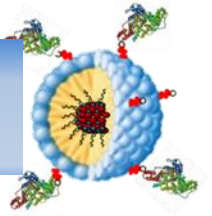
The shift of emission maximum wavelength from 560 nm to 532 nm assigned to the micellar environment around the probe, which is particularly sensitive to any polarity change of the surrounding medium



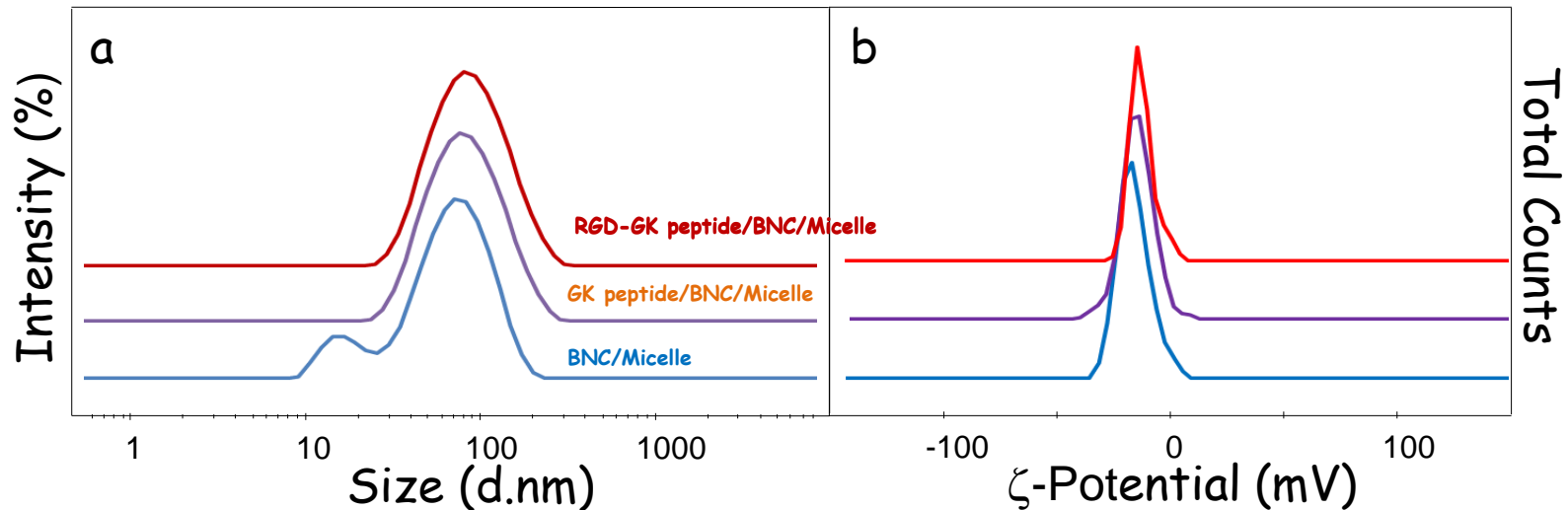
The presence of Amide I mode band in the peptide/BNC/Micelle spectrum confirms the occurrence of the bioconjugation reaction.

Valente G., Depalo N., de Paola I., Iacobazzi R. M., Denora N., Laquintana V., Comparelli R., Altamura E., Latronico T., Altomare .M., Fanizza E., Striccoli M., Agostiano A., Saviano M., Del Gatto A., Zaccaro L. and Curri M. L., Nanoresearch, 2016, 644-662.

Dynamic Light Scattering



monomodal size distribution



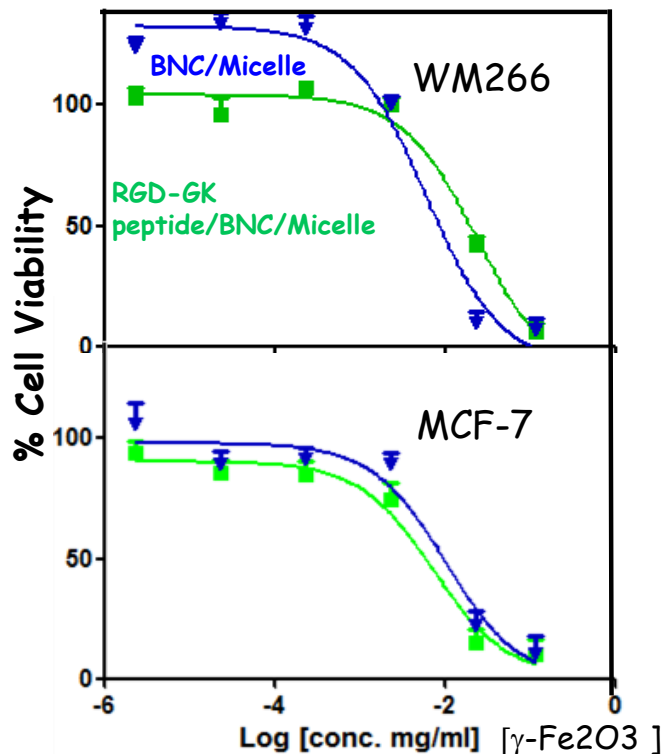
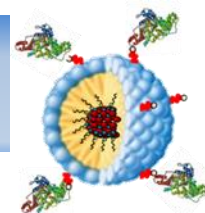
81 nm (PDI = 0.108 ± 0.003)

80 nm (PDI = 0.188 ± 0.002)

-17.1 ± 0.9 mV

-16.6 ± 0.26 mV

Citoxycity studies



| Cell Line | IC50 (mg/ mL) | |
|-----------|-----------------|---|
| | BNC/Micelles | RGD(GK)2 - Peptide/BNC/Micelle Conjugates |
| MCF-7 | 0.0095 ± 0.0020 | 0.0055 ± 0.0032 |
| WM266 | 0.0076 ± 0.0030 | 0.0190 ± 0.0027 |

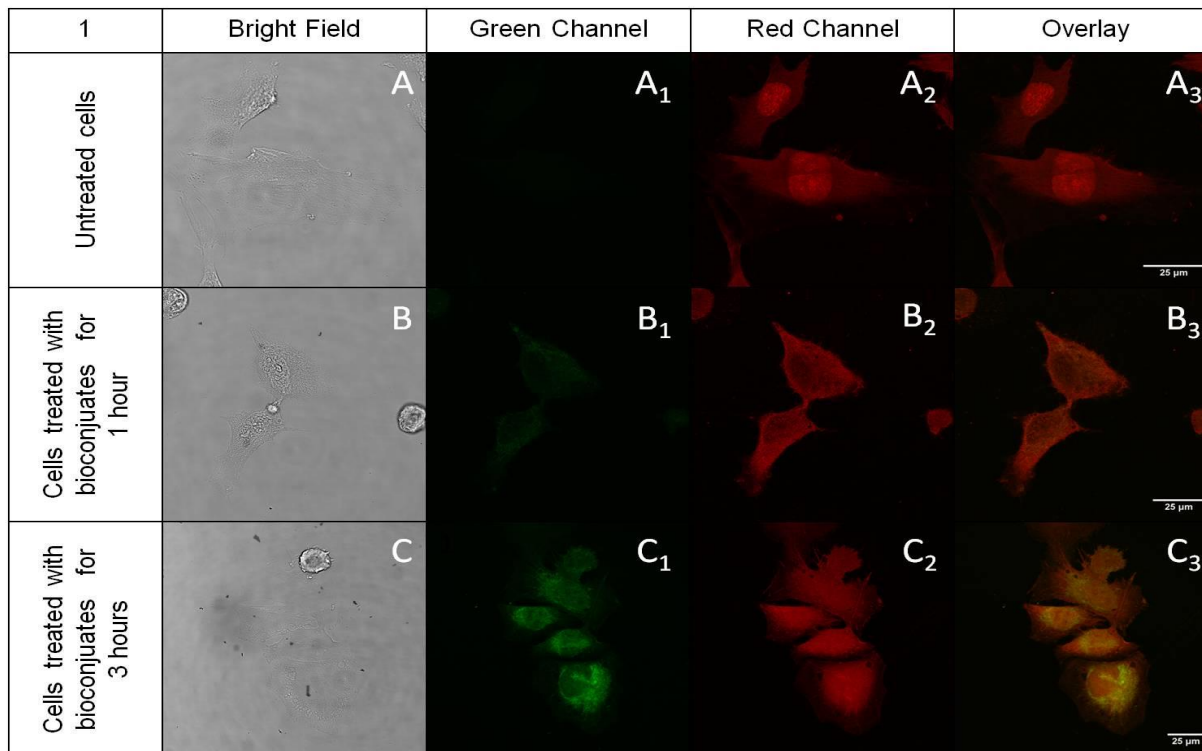
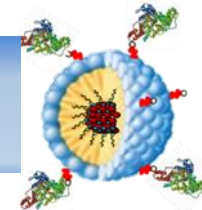
IC50 values expressed as γ -Fe₂O₃ concentration. In WM266 cells the cytotoxic activity of RGD(GK)2/BNC/Micelle conjugates has been found slightly lower than that of BNC/Micelles

Incubation with γ -Fe₂O₃ concentration values ranging from 2.27*10⁻⁶ to 0.113 mg/mL (TiO₂ concentration range from 2.93*10⁻² to 5.87*10⁻⁷ mg/mL) for 72 hours.

At γ -Fe₂O₃ concentration values ranging from 2.27*10⁻⁶ to 2.27*10⁻⁴ mg/mL no significant effect on cell viability can be observed

Valente G., Depalo N., de Paola I., Iacobazzi R. M., Denora N., Laquintana V., Comparelli R., Altamura E., Latronico T., Altomare M., Fanizza E., Striccoli M., Agostiano A., Saviano M., Del Gatto A., Zaccaro L. and Curri M. L., Nanoresearch, 2016, 644-662.

Confocal microscopy

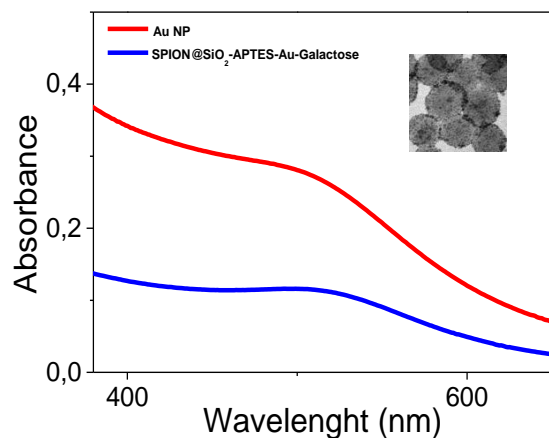
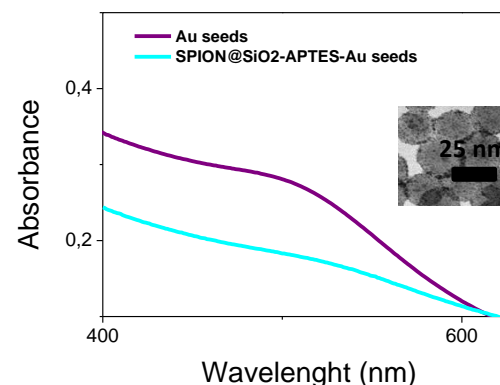
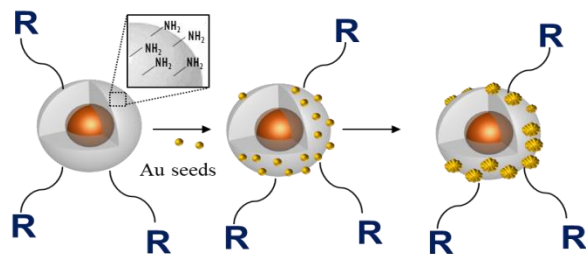
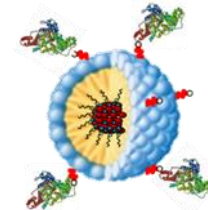


The cells have been incubated with conjugate samples at concentration of $2.27 \cdot 10^{-3}$ mg/mL for 1 and 3 hours fixed and treated with Phalloidin-TRIC, able to stain the F-actin cytoskeleton of the cell.

Scale bar 25 μ m

Valente G., Depalo N., de Paola I., Iacobazzi R. M., Denora N., Laquintana V., Comparelli R., Altamura E., Latronico T., Altomare M., Fanizza E., Striccoli M., Agostiano A., Saviano M., Del Gatto A., Zaccaro L. and Curri M. L., Nanoresearch, 2016, 644-662.

Silica coated SPION decorated with Au seeds



asialoglycoprotein receptor tumor marker
overexpressed in hepatocarcinoma

